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In Vitro and in Vivo investigation on stem cells isolated from pulp and gingival tissues from periodontally compromised teeth.

Doctoral Dissertation of:
Rodolfo Mauceri

Supervisors:

Prof. Silvio Abati

Prof. Michele Mignogna

Tutor Unipa:

Prof. Giuseppe Pizzo

Tutor UAntwerpen:

Prof. Christian Rolfo

Prof. Olivier Vanderveken

The Chair of the Doctoral Program:

Prof. Giuseppina Campisi

Years 2014/2016 - Cycle XXIX



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INDEX

1. Abstract	Pag 2
2. Summary	Pag 3
3. CHAPTER 1 Background, Rationale and Objectives	Pag 5
4. CHAPTER 2 Materials/Patients and Methods	Pag 10
5. CHAPTER 3 Results	Pag 17
6. CHAPTER 4 Discussion	Pag 21
7. CHAPTER 5 Tables and Figures	Pag 24
8. Bibliography	Pag 36
9. Scientific Products (bound)	Pag 43

Abstract

Tissue engineering (TE) and regenerative medicine are interdisciplinary fields that provide new regenerated tissues by the development of biological substitutes that restore, maintain and or improve tissue function.

Dental pulp stem cells (DPSCs) and gingival mesenchymal stem cells (GMSCS) are a valuable source of stem cells for bone tissues regeneration.

The main objective of the present study is to evaluate the ability of DPSCs and GMSCs harvested from periodontally-affected teeth to produce *in vitro* and *in vivo* new mineralized bone tissue, in comparison to healthy teeth.

Weefsel engineering (TE) en regeneratieve geneeskunde zijn interdisciplinaire vakgebieden die samen zorgen voor weefselregeneratie door de ontwikkeling van biologische alternatieven die de weefselfunctie herstellen, onderhouden en verbeteren.

Dentale pulpa stamcellen (DPSCs) en gingivale mesenchymale stamcellen (GMSCs) zijn waardevolle bronnen voor stamcellen voor botweefsel regeneratie.

Het hoofddoel van de huidige studie is om de capaciteit na te gaan van deze DPSCs en GMSCs, geoogst uit periodontaal aangetaste tanden, om *in vitro* en *in vivo* nieuw gemineraliseerd botweefsel te produceren, in vergelijking met gezonde tanden.

Summary (Informative Abstract)

Dental pulp stem cells (DPSCs) and gingival mesenchymal stem cell (GMSCs) represent an alternative source of mesenchymal stem cells, their features make them ideal for bone tissue engineering. In this study, we verified the ability of DPSCs and GMSCs harvested from periodontally compromised teeth to produce *in vitro* and *in vivo* new mineralized bone tissue, in comparison to healthy teeth.

Initially, we isolate DPSCs and GMSCs from dental pulp and gingiva harvested from patients suffering of severe periodontitis (Test group) and from healthy patients (Control group). To characterize DPSCs and GMSCs colony-forming assay and cytofluorimetric and mRNA real time quantification analysis were performed. The effects of pro-inflammatory cytokines on MSC cell proliferation and differentiation potential were investigated. Furthermore, we investigated the capability of DPSCs and GMSCs to colonize Poly-L-lactic Acid (PLLA) scaffolds, produced by mean of Thermally Induced Phase Separation technique (TIPS). Finally, we investigate the capability of DPSCs and GMSCs from both studied groups to induce bone formation *in vivo*.

Our findings provide evidence that tissue (both pulp and gingiva) from periodontally-compromise teeth can be used as source of MSCs with intact stem properties and increased differentiation potential. Pro-inflammatory cytokines activate a cytoskeleton remodeling by recruiting heat shock proteins (HSPs) including HSP90, HSPA9, thioredoxin-1 and actin-depolymerizing factors (ADFs) as profilin-1, cofilin-1 and vinculin that probably mediated the advantage acquisition in inflamed environment. Moreover, the DPSCs and GMSCs have been shown the capability to colonize successfully the PLLA scaffolds, but, in the animal study group, we did not observe new bone formation. Indeed, new *in vivo* studies are ongoing: PLLA scaffolds with DPSCs or GMSCs were implanted, in order to provide a more stable osteoinductive and osteoconductive structural support.

Dentale pulpa stamcellen (DPSCs) en gingivale mesenchymale stamcellen (GMSCs) vertegenwoordigen een alternatieve bron voor mesenchymale stamcellen. De eigenschappen van deze celtypes maken hun tot ideale kandidaten voor botweefsel engineering. In deze studie gingen we na of DPSCs en GMSCs, geoogst uit periodontaal aangetaste tanden, in staat zijn om *in vitro* en *in vivo* nieuw gemineraliseerd botweefsel te genereren, in vergelijking met gezonde tanden.

Eerst isoleerden we DPSCs en GMSCs uit de dentale pulpa en gingiva van patiënten die leden aan ernstige periodontitis (test groep) en gezonde patiënten (controle groep). Om deze DPSCs en GMSCs te karakteriseren voerden we de kolonie-vormende assay, cytofluorimetrische en mRNA real-time

kwantificatie analyses uit. Vervolgens werden de effecten van pro-inflammatoire cytokines op de proliferatie en differentiatie van MSC cellen onderzocht. Verder onderzochten we de capaciteit van DPSCs en GMSCs om Poly-L melkzuur (PLLA) substraat te koloniseren, dat geproduceerd werd door de thermaal geïnduceerde fasescheidingstechniek (TIPS). Tenslotte onderzochten we de capaciteit van DPSCs en GMSCs van beide studiegroepen om botvorming te induceren in vivo.

Onze resultaten bewezen dat weefsels (zowel uit de pulpa als uit de gingiva) uit periodontaal aangetaste tanden gebruikt kunnen worden als een bron voor MSCs met intacte stamceleigenschappen en verhoogd differentiatiepotentieel. Pro-inflammatoire cytokines activeren een cytoskelet herschikking door hiteschok eiwitten (HSPs) te rekruteren, zoals HSP90, HSPA9, thioredoxin-1 en actine-depolymeriserende factoren (ADF) zoals profilin-1, cofilin-1 en vinculin die waarschijnlijk de voordelen van een inflammatoire omgeving regelen. Bovendien vertoonden DPSCs en GMSCs de capaciteit om met succes PLLA substraten te koloniseren, maar in de dierlijke studiegroep hebben we geen nieuwe botformatie geobserveerd. Nieuwe in vivo studies worden momenteel uitgevoerd: PLLA substraten die DPSCs of GMSCs bevatten, werden geïmplanteerd om meer stabiele osteoïnductieve en osteoconductieve structurele steun te bieden.

Background, Rationale and Objectives

1.1 Restoring missing teeth and bone resorption

Missing teeth and supporting oral tissues have traditionally been replaced with dentures or bridges permitting restoration of chewing function, speech, and aesthetics^{1,2}.

In the last decades, the use of dental implants has been increasingly applied to replace the missing teeth; indeed, today, dental implants are defined as the first-choice treatment modality for replacing missing teeth^{3,4}.

Historically, osseointegration was firstly described by Branemark 1977 and is defined as the direct structural and functional connection between living bone and implant surface^{5,6}. The achievement and the maintenance of osseointegration is linked with implant stability, essential for successful long-term results^{7,8}.

Implant stability is obtained mechanically during the insertion of the fixture in the jawbones; subsequently, the bone remodelling around the implants create a direct structural and functional connection between living bone and implant surface^{6,8,9}.

A sufficient bone volume to achieve primary implant stability is needed to place dental implants; however, bone resorption is a pathophysiological process induced by many mechanisms.

Primarily, the main cause of jawbone resorption is related to tooth loss, other factors that may influence the bone anatomy are trauma, surgery or congenital malformation. In particular, Dental caries and periodontal disease are the major causes for tooth loss¹⁰⁻¹².

1.2 Bone regeneration procedures

Successful repair of bone deficiencies is a major concerning topic in the oro-maxillo-facial (OMF) field. To restore the bone tissue volume is challenging because oro-facial functions, such chewing and swallowing, are delicate, due to the complex anatomical structures of the jawbones and the oral mucosa^{3,13-15}.

Guided bone regeneration (GBR) procedures have become everyday treatment in order to allow the placement of dental implants or the periodontal regeneration; GBR is based on the application of membranes and grafting materials^{16,17}.

To achieve a successful GBR, there are various indications, different alternative techniques, and numerous 'biologically active' agents and biomaterials currently used in dental practice¹⁶⁻¹⁹.

Mostly of GBR techniques require special barrier membranes to protect defects from the ingrowth of soft tissue cells so that bone progenitor cells may develop bone uninhibited. Membranes can be resorbable or non-resorbable; resorbable are usually made by polylactic acid (PLA) or L-polylactic acid (PLLA), porcine collagen or polyglactin. Non-resorbable membranes are usually made by titanium-reinforced expanded polytetrafluoroethylene (e-PTFE)²⁰.

Among the graft materials there are more options, autogenous bone grafts are considered to be the material of choice for GBR, indeed it is defined as the "gold standard", as it has the biocompatibility, osteoinductive and osteoconductive properties, without immunological reactions and extra costs for purchasing biomaterials²¹⁻²³. However, their use leads to an additional surgical intervention, possible complication of the donor site and a limited amount of graft²¹⁻²³.

Other bone substitutes are: allografts, xenografts or alloplastic graft materials.

Both of these three substitutes possess advantages and disadvantages, and they can be used in combination with autografts or alone, according to the chosen GBR technique^{17,19,22}.

1.3 Tissue Engineering and Regenerative medicine

Tissue engineering (TE) and regenerative medicine (RM) are emerging fields focused on the development of alternative strategies for tissue or organ repair that made significant progress in the last years^{24,25}.

TE provide new regenerated tissues by the appliance of cells, scaffold and growth factors, alone or in combination; nowadays RM has made exceptional progress leading to the regeneration of numerous organs and organ systems by using the capability of stem cells to differentiate into specialized cell types²⁶⁻²⁸.

Stem cells are promising tools for tissue repair, due to their extensive proliferation and differentiation plasticity, unique ability that make them able, in theory, to regenerate injured tissues^{24,29}.

Stem-cell-based bone tissue engineering has demonstrated potential; the ideal cell populations are autologous mesenchymal stem cells (MSCs) from adult sources³⁰.

Defined as a population of non-hematopoietic fibroblast-like cells, MSCs are a self-renewing populations which express the ability to differentiate into multiple lineages, including osteoblasts, adipocytes and chondrocytes^{24,31,32}.

The main difficulties of the use of MSCs remains the identification of accessible sites within the human body where can be collected an adequate amount of stem cells. Indeed, the number of MSCs is higher before the birth, but it decreases during the aging, reducing their presence in several "niches"^{24,31,32}.

MSCs they have been usually isolated from bone marrow and are defined as bone-marrow-derived mesenchymal stem cells (BM-MSCs), but the BM-MSCs possess some weakness, such as their difficulty of isolation, large trauma, high expense, and patient's low degree reception^{33,34}.

Recently, many niches of MSCs have been described in the oral cavity: the dental pulp from permanent (DPSCs) or deciduous teeth (SHED), the periodontal ligament (PDL), the apical papilla, the dental follicle and the gingival tissue (GMSCs)³⁵⁻³⁹.

1.4 Dental pulp stem cells

DPSCs have been described for the first time by Gronthos et al in the 2000, which described the presence of neural crest-derived stem cells from the dental pulp of adult human body³⁵.

Neural crest-derived stem cells originate from the process that give rise to the dental laminae during the sixth week of the embryogenesis, when the ectoderm begins to proliferate. The ectoderm-mesoderm interactions lead to the development of tooth germs, where neural crest cells differentiate into the dental organ, dental papilla and dental follicle.

Consequently, dental pulp develops from both ectodermic and mesenchymal components, containing neural crest cells. These adult stem cells have been called DPSCs, when isolated from permanent teeth; while, when isolated from deciduous teeth, they are defined SHEDs (Stem Cells from Human Exfoliated Deciduous)²⁶.

As well as MSCs, DPSCs and SHEDs are clonogenic cells capable of both self-renewal and the capability to give rise to different specialized cell types⁴⁰.

Moreover, compared to the BM-MSCs, DPSCs and GMSCs are easier to be harvested and have demonstrated the ability to proliferate faster, to be mostly homogenous and to have excellent capacity to differentiate in osteogenic cells^{33-35,40}.

Indeed, since their first isolation, DPSCs and SHEDs have been widely investigated for their potential application in TE in the last decades; in vitro and in vivo results have shown the capability of these stem cells not only in bone tissue, but also in adipose tissue, dentin-like tissue, cartilage, hair bulb, nerves fibres⁴⁰. In particular, DPSCs and SHEDs have been successfully applied for bone regeneration not only in animal models but also in human being⁴¹⁻⁴³.

In addition, the presence of DPSCs have been investigated from tissues harvested from fractured teeth, teeth with caries or irreversible pulpitis, or aggressive periodontitis⁴⁴⁻⁴⁷.

1.5 Gingival mesenchymal stem cells

Gingival tissue is composed of an epithelial layer and underlying lamina propria; as well as dental pulp and all the other craniofacial tissues of mesenchymal origin, these tissue develops from the cranial neural crest⁴⁸.

Gingival mesenchymal stem cells (GMSCs) have been isolated more recently than DPSCs, indeed, GMSCs were firstly described by Zhang et al. in 2009⁴⁹.

The GMSCs are a subpopulation of the gingival fibroblast and exhibited all the MSCs characteristics: self-renewal capability, multipotent differentiation, and immunomodulatory abilities both in vitro and in vivo^{49,50}.

It has been demonstrated that GMSCs are more superior to BM-MSCs: GMSCs are uniformly homogenous, proliferate faster than BM-MSCs without any growth factor, display stable phenotype, maintain normal karyotype and telomerase activity, and are not tumorigenic⁵¹⁻⁵³.

Clinically, it is extremely simple to collect gingival tissue by biopsy, contrary to pulpar or periodontal cells that require tooth extraction for harvest^{50,52}. Furthermore, the regeneration of gingival anatomy usually takes place in a short time period after wounding, usually lead to a perfect healing of the gum without complication for the patients, representing another advantage^{50,52}.

Similar to other MSCs, GMSCs cultures can be induced to differentiate into osteo-, adipo- and chondrogenic lineages as well as to myofibroblasts in vitro⁵⁴. Noteworthy, experimental studies have proved that GMSCs possess also the capability to develop mineralized tissues in vivo⁵⁵⁻⁵⁷.

In addition, as well as for the DPSCs, the presence of GMSCs has been proved also in inflamed and hyperplastic tissues^{53,58}.

1.6 Scaffolds

Not only the source of the cells is important but also the design and the formation of a structure able to support the migration and growth of cells is essential to achieve new tissue formation^{25,59}.

To achieve bone tissue regeneration is needed the use of a suitable scaffolds; the major function of scaffolds is to furnish temporary structural support for osteoprogenitor cells, and osteoinductive factors desired to repair bone defect^{25,59}.

Scaffolds are principally biodegradable, synthetic, three dimensional (3D) structures, emulating the extracellular matrix and containing macro- and micro-pores that guide cell adhesion, proliferation and differentiation^{60,61}.

To secure a high density of colonizing cells and to promote neovascularization when implanted in vivo, the scaffolds should possess excellent mechanical properties, extensive surface area and pore size distribution along with highly interconnected porous structure^{62,63}.

Thermally induced phase separation (TIPS) can be used to produce a well interconnected porous scaffold; indeed, this technique allows to obtain different porous materials as scaffold architectures simply changing one or more experimental processing parameters and system properties^{61,64}.

“TIPS technique is based on thermodynamic demixing of a homogeneous polymer-solvent solution into a polymer-rich phase and a polymer-lean phase, usually by either exposure of the solution to another immiscible solvent or cooling the solution below a binodal solubility curve”⁶⁴.

Various polymers have been employed to create scaffolds by mean of TIPS technique; Poly(L-lactide) (PLLA) has been extensively used as a scaffold material for bone tissue engineering due to its superior mechanical properties, well-known biodegradability and biocompatibility⁶⁵⁻⁶⁷.

1.7 Aim

The aim of the study is to provide the evidence of a new potential sources of MSCs for bone regeneration in dentistry. The DPSCs and the GMSCs were isolated from periodontally compromised teeth and their corresponding inflamed gingiva (P-DPSCs and P-GMSCs).

The inflammatory effects on human dental stem cells has been evaluated; we compared the MSCs markers, MSCs gene profile, proliferation and in vitro differentiation ability of the P-DPSCs and P-GMSCs compared to healthy teeth (H-DPSCs and H-GMSCs). We investigated if pro-inflammatory microenvironment negative affects dental MSCs characteristics and their capability and we speculated about a closer link between chronic inflammation and bone formation.

Furthermore, we evaluated the capability of P-DPSCs and P-GMSCs to develop vital bone tissue in vivo, in comparison to H-DPSCs and H-GMSCs.

In addition, P-DPSCs and P-GMSCs, as well as H-DPSCs and H-GMSCs, have been seeded on 3D PLLA scaffolds obtained with the TIPS technique to study their ability to form new mineralized bone tissue in vitro.

Materials and Methods

2.1 Ethics

All the procedures reported were approved by the Internal Ethical Committee of the University Hospital A.U.O.P “P. Giaccone” of Palermo (Internal registry: 5/2014). Patients signed an informed consent form before recruitment for the study.

2.2 Dental pulp and gingival tissue extraction

Dental pulp was extracted from teeth of healthy adults aged 18-75 years.

The eligibility criteria for participants were the following: extraction needed for molars suffering from severe periodontal disease (mobility grade III) (Test group), extraction needed for wisdom teeth for orthodontic reasons (Control group), no suspected or visible pregnancy in females, positive response to the vitality test performed on teeth to be extracted.

Before extraction, each patient had to rinse his or her mouth with 0.2% chlorhexidine for one minute (Meridol®, Gaba Vebas S.r.l., Rome, Italy) to decontaminate the oral cavity. Gingival tissue was collected while the patient underwent oral surgery procedures for tooth extraction.

2.3 Establishment of pulp dental and gingival cell cultures

All the samples were processed by Professor Giordano’s research group (Laboratory of Regenerative Medicine (DIBIMIS)).

After surgery the pulpal or the gingival tissue was transferred to an RPMI culture medium (Sigma - Aldrich, Milano, Italy) enriched with 0.2 mg/ml gentamicin, 0.25 mg/ml levofloxacin, 0.10 mg/ml vancomycin, 0.25 mg/ml fluconazole in a 50 ml tube and within 24 hrs the samples were digested.

Digestion was carried out in a solution of 5 mg/ml collagenase G (Abiel, Palermo, Italy) and 2 mg/ml collagenase H (Abiel, Palermo, Italy), 4:1 respectively, 4 hrs at 37°C, in agitation. The digests containing primary cells from the pulp or the gingiva were centrifuged and transferred to a T25 cell culture flask (EuroClone, Milano, Italy) or a p60 dish culture (to which we referred as passage 0, p0). The cells were maintained in culture in RPMI culture medium enriched with 0.5µg/ml gentamicin, 0.25µg/ml levofloxacin, 0.10µg/ml vancomycin, 0.25µg/ml fluconazole and 5% fetal bovine serum

and incubated at 37°C, in 5% of CO₂. Primary cells were attached to the flask within 4-5 days. Once they reached 80% of confluence (in about two weeks) they were trypsinized and the subculture was started (passage 1, p1). By subculture p4 the antibiotic and anti-fungal cover was abolished (Expansion Medium: EM). The p1–p8 cells were used for the in vitro assays.

2.4 Colony-forming assay

To assess the colony-forming efficiency of the dental pulpal mesenchymal stem cells (DPSCs) and gingival mesenchymal stem cells (GMSCs), single-cell suspensions (p0) from the periodontally-compromised teeth and healthy donors were seeded in a six-well culture in RPMI with 10% FBS at a density of 300 cells/well and cultured at 37°C and in 5% of CO₂. After 14 days, the cells were fixed in 4% paraformaldehyde, stained with 0.1% crystal violet. Only the cellular groups containing more than 50 cells were considered as colonies.

2.5 Cell proliferation curve and Population Doubling (PD)

Proliferation was assayed by Trypan blue (Sigma-Aldrich), according to the manufacturer's instructions. The p2 GMSCs or p2 DPSCs from Healthy (H) or Periodontally-compromised (P) donors were seeded at a density of 4x10³ cells/cm². The p4 H-DPSCs or p4 H-DGMSCs with or without 20ng/ml IL-1 β and 40ng/ml TNF- α were seeded in a 96-well culture at a density of 4x10³ cells/cm² cells and cultured up to 120 hours. The cell counts were performed by optical microscope observation after trypan blue staining every 24 hours during the incubation period. The doubling time (DT) was calculated according to the literature data (Roth V. 2006 on the website <http://www.doubling-time.com/compute.php>). Three sets of experiments for each sample were used for calculations.

2.6 Cytokine toxicity assay

The p4 H-GDPSCs or p4 H-DGMSCs with or without 20ng/ml IL-1 β and 40ng/ml TFN- α were seeded in a 96-well culture at a density of 4x10³ cells/cm² cell and cultured for up to 72 hours. Cell viability was evaluated by UV absorption spectrum at 550 nm at 24, 48 and 72 hours using a micro-plate reader, after 3-(4,5-Dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide (MTT) incubation for 4 hours at 37°C. Bone Marrow-derived Mesenchymal Stem Cells (BM-MSCs) were used as positive control.

2.7 Cell cycle cytofluorimetric analysis

Single cell suspensions of H-DPSCs, P-DPSCs or H-GMSCs and P-GMSCs were obtained and DNA content analysis was performed, according to Nicoletti's protocol. Briefly, 1x10⁶ cells were fixed in 70% ethanol, rehydrated in PBS and then resuspended in a DNA extraction buffer (with 0.2 M NaHPO₄, 0.1% Triton X-100 and, pH 7.8). After staining with 1 μ g/ml of propidium iodide (PI) for 5 minutes, fluorescence intensity was determined with a FACS Calibur flow cytometer (Becton-Dickinson, New Jersey, USA). Data acquisition was performed with CellQuest (Becton Dickinson)

software, and the percentages of G1, S, and G2 phase cells were calculated with the MODFIT-LT software program (Verity Software House, Inc.). The Proliferation index (PI) was expressed as % G2 + % M.

2.8 Surface marker cytofluorimetric analysis

The H-DPSCs, P-DPSCs or H-GMSCs and P-GMSCs were harvested and filtered through a 40µm filter mesh and suspended at the concentration of 1x10⁶ cells/ml. Then 100 µl of cell suspension containing 5x10⁵ cells were used for each cytofluorimetric test.

2.9 Flow cytometric Immunophenotyping

Human anti-HLA-DR, human anti-CD34, human anti-CD45 monoclonal antibodies were tested on H-DPSCs, P-DPSCs or H-GMSCs and P-GMSCs and were detected with the appropriate secondary antibody (Table 1). The incubation conditions were in accordance with the manufacturer's instructions. Unstained cells were used as a negative control. BM-MSCs were used as a positive control.

2.10 Stem cell phenotype

The cells were tested for expression of Stro-1, CD146 and CD29 and SSEA4 surface MSC markers, with the appropriate human anti-monoclonal antibody. The antibody dilution, incubation and detection conditions are shown in Table 1.

All reaction mixtures were then acquired with a FACS Calibur flow cytometer (Becton-Dickinson, New Jersey, USA) and analyzed with the CellQuest Pro software. Unstained cells were used as negative control.

Isolation of total RNA, Reverse-PCR, Real Time PCR and semi-quantitative PCR Total RNA was extracted and purified using the E.Z.N.A. Total RNA Kit I (Omega Bio-Tek Inc Georgia, USA) according to the manufacturer's instructions. RNA quantity and quality were assessed using Nano Drop 2000 (Thermo Scientific); 2µg of MSC total RNA were reverse-transcribed to cDNA in a volume of 20µl with Oligo dT primers (Applied Biosystems, California, USA) and the Reverse Transcriptase Rnase kit (Improm II, Promega, Wisconsin, USA).

2.11 Real-time quantitative PCR (qRT-PCR)

qRT-PCR primers were purchased from Qiagen (QuantiTect® Primer Assays, Qiagen, Milan, Italy) and Eurofin MWG (Biotech, Germany) and are listed in Table 2. All reactions were performed using the Quantitect SYBR Green PCR Kit (Qiagen, California, USA) using the RotorGene Q Instrument (Qiagen, California, USA). Each cDNA sample was mixed with specific primer sets and PCR master mix. The PCR reactions were performed using the following parameters for 40 cycles: denaturation at 95°C for 3 minutes, 95°C for 20 seconds, annealing at 60°C for 30 seconds and elongation at 72°C for 60 seconds. Reactions were performed at least in triplicate. The specificity of the amplified products

was determined by the melting peak analysis. The relative quantification model with efficiency correction was applied to normalize the expression of the target gene to β -actin (used as a housekeeping gene) and to compare gene expression with BM-MSCs (used as a positive cell control), on Rest2009 software (Relative Expression Software Tool, Qiagen)³³. The results were described as histograms using the GraphPad Software, Inc., California.

qRT-PCR analysis for the stem genes was also performed after pro-inflammatory cytokine treatment: H-DPMSCs or H-GMSCs were incubated with 20ng/ml IL-1 β and 40ng/ml TNF- α up to 72 hours. The forward (F) and reverse (R) primer sequences used for the reactions of amplification are listed in supplemental materials (Table 2).

2.12 Semi-quantitative PCR

To determine the expression of runx-2 (Runt-related transcription factor 2) and actin-depolymerizing factors (ADFs): 1 μ l complementary DNA was added to a 50 μ l reaction containing 5 μ l 10x reaction buffer, 50mmol/L MgCl₂, 1 μ l dNTPs, 50pmol sense and anti-sense primers and 0.5 U Taq Gold DNA polymerase. The reactions were carried out according to the following protocol: I) 95°C for 10 minutes, II) 35 cycles at 95°C for 45 seconds, III) primer-specific annealing temperature for 45 seconds, IV) 72°C for 45 seconds, V) a final extension cycle at 72°C for 7 minutes, followed by a termination cycle at 4°C.

The primers were purchased by MWG and the sequences were the following: runx-2 F: 5'-TACGACTGGACGCTGGTGC-3', R: 5'-TTCATGGGTCGCTTGACGT-3'; Profilin-1 (Pfn-1) F: 5'-ACCCGAAACAAGAAGAC-3', R: 5'-ACTGGTCCGATAACCTCCCA; Cofilin-1 (Cfl-1) F: 5'-TGCGGCTCCTACTAAACGG-3', R: 5'-ACGCACCTTCATGTCGTTGA-3'; Vinculin (Vcl) F: 5'-ATGTCTCCTATATCCTGGTTTTTGT-3', R: 5'-GCAGGAAGTGCCTTCAGAC-3'

The protein-interaction networks (PIN)

Network analysis was performed on the heat shock proteins (HSPs) and ADFs using the STRING (Search Tool for the Retrieval of Interacting Genes/Proteins) found at the website <<http://string-db.org/>>.

2.13 Bone in vitro formation

5x10³/cm² H-DPSCs or H-GMSCs were incubated in EM with 20ng/ml IL-1 β and 40ng/ml TNF- α (cytokine precondition treatment). After 72 hours the medium was replaced with homemade osteogenic differentiation medium (ODM). 5x10³/cm² H-DPSCs, P-DPSCs or H-GMSCs and P-GMSCs were cultured in ODM. After 21 days of culture in the ODM, the cells were stained with Alizarin Red S (Sigma-Aldrich, St. Louis, USA) to detect calcium deposits. Briefly, the medium was removed and the cells were fixed with 4% formaldehyde solution for 30 minutes, and after fixation rinsed twice with distilled water and stained with 2% Alizarin Red S (pH 4.2) for 3 minutes. After observation under a light optical microscope, the images were acquired by Nikon DS-fi1 cam and for quantification of the

calcium deposits ImageJ software was used (<https://imagej.nih.gov/ij/docs/concepts.html>). The ODM consisted of DMEM supplemented with 15% FBS, 10⁻⁴ mM dexamethasone (Sigma-Aldrich, St. Louis, USA), 10 mM glycerophosphate (Sigma-Aldrich, St. Louis, USA) and 0.05 mM ascorbic acid (Sigma-Aldrich, St. Louis, USA)²⁴.

2.14 PLLA Scaffold preparation

The Poly-L-lactic Acid (PLLA) scaffolds were produced by Professor Brucato's research group (Department of Civil, Environmental, Aerospace, Materials Engineering (DICAM) of the University of Palermo).

Thermally Induced Phase Separation technique (TIPS) was employed in order to produce well interconnected porous structure, following procedures already reported in literature^{64,68}.

A homogeneous ternary solution composed of PLLA, dioxane and deionised water was prepared with a constant dioxane to water ratio of 87/13 (wt/wt); the polymer concentration was chosen to be 4% (wt/wt). The cloud point of the solution was at 40°C, so the solution was initially kept at 60°C.

In order to establish the ideal porous structure for the DPSCs e GMSCS cells, different scaffold were prepared with different thermodynamic pathways and related different microporous structures.

All the scaffolds were prepared using a cylinder aluminium sample holder (diameter 6 mm, height 30 mm).

The first two types of scaffolds were prepared using a binodal de-mixing technique; first the solution was hot poured into the sample holder, then the sample holder was immersed into a thermostatic water bath, in order to suddenly decrease the temperature to 30°C (scaffold a) or 25 °C (scaffold b) for 15 min (de-mixing time),

Subsequently, in order to freeze the as-obtained structures, a quench by pool immersion in an ethyl alcohol bath at a temperature of -20°C for 15 min was performed. Then, the scaffolds were extracted from sample holder, washed into deionised water for 24h and dried at 20°C under vacuum overnight, in order to completely eliminate any solvent trace.

The microporous structure of the obtained scaffolds were approximately 150 µm (scaffold a) and 50-70 µm (scaffold b).

After the initial in vitro studies, a different protocol was adopted consisting of a spinodal decomposition technique (scaffold c). This procedure was slightly different from the first described before. After that the sample holder was filled with the ternary solution, it was immersed into a thermostatic water bath at 0°C for 10min; afterwards a teflon coating was applied and the as-obtained structure was cooled in an ethanol bath at -20°C for 15 min. The as-obtained structure were then washed and dried as described before. With this second technique achieved scaffolds with 5-20 µm micropores were achieved.

2.15 Scaffold characterization before seeding

Due to the cylindrical shape of the sample holder, the cylindrical 3D scaffolds were cut to obtain disks of a diameter of 6 mm and thickness of 2 mm.

The disks were sterilized in 70% ethanol (v/V) solution under vacuum for 18 h; subsequently four washes were carried out using with sterile PBS, to remove all the ethanol.

A solution of collagen (type I solution from rat tail,) in acetic acid (0.02N) at the concentration of 200µm/ml was prepared to coat the scaffolds, the solution was filtered with 0,2 µm filters.

To achieve the collagen coating, the scaffolds were immersed in the obtained solution for 90 min at 37°C. Afterwards the scaffolds were washed with PBS and kept in culture medium until the cell seeding.

2.16 GMSCs seeding

To test the capability of the MSCs chosen in this project, initially it was decided to employ only the P-GMSCs.

The in vitro test was conducted by seeding a cell suspension, at density of 1×10^5 GMSCs, on the top of scaffolds a and b (respectively with 150 and 50/70 µm micropores).

After the seeding the scaffolds were incubated at 37°C for 90 min without the culture medium to promote the cell adhesion; then the scaffolds were placed into 24-well plates and 1ml of complete DMEM was added. Incubation was left at 37°C and 5% of CO₂.

The same procedures were applied to test the scaffolds c; regarding this second in vitro examination, two different volume of the solution containing the P-GMSCs were used: 20 µl and 15 µl.

Viability of the P-GMSCs was investigated at established points (after 12h, 40h and 120h).

2.17 Cell Counting Kit-8 assay

The Cell Counting Kit-8 (CCK-8) assay was utilized to detect the viability of P-GMSCs seeded on scaffolds a and b. The scaffolds were placed in 96-well plates, and the absorbance at 450 nm was detected at 1–6 days after seeding.

2.18 Alamar Blue cell viability assay

The scaffolds c were transferred into new 24-well plates with 500 µl of Alamar Blue solution and DMEM, then plates were incubated for 3h at 37°C.

Then the solution incubated with the scaffolds was transferred in a 96-well plates (100 µl) and the fluorescence was evaluated by a spectrophotometer.

2.19 Cell vitality assay

To test the cell vitality assay of scaffolds c were used Acridine orange (AO) and ethidium bromide (EB). The dye mix for the EB/AO staining was 100 µg/ml acridine orange and 100 µg/ml ethidium bromide in PBS.

The scaffolds tested were firstly placed in new 24-well plates and washed four times with PBS (100 μ l), every wash cycle was of 5 minutes by mean of an oscillating surface.

EB/AO dye mix (30 μ l) was added to each well for 5 min, and cells were viewed under the fluorescence microscope using FITC and TRITC filters.

2.20 DAPI assay

The investigated scaffolds were placed in 24-well plates and washed three times with PBS (100 μ l); then the scaffolds were fixed in 3,6% formaldehyde in PBS for 15 minutes. After washing in PBS, samples were stained with 1:100 μ l DAPI in PBS for 1 minute, finally the scaffolds were observed under the fluorescence microscope.

2.21 In vivo implantations

All experimental procedures and protocols were approved by the “OPBA – Organismo Preposto al Benessere degli Animali” of the “A.Mirri” Experimental Zooprophyllactic Institute of Sicily (approval No. 1061/2015) and by the Italian Minister of Health (approval No.1185/2015).

All the surgical procedures were performed at the “A.Mirri” Experimental Zooprophyllactic Institute of Sicily.

6-week-old immunodeficient nude mouse (NU/NU) were used for the study, in each mouse were injected subcutaneously on the dorsal surface (n=2 per mouse) the cells suspension (fig.1).

In detail, in the first trial, approximately 10^5 cells of DPSCs or GMSCs from healthy and periodontal donors were suspended in 100 μ l of differentiation medium, for each group were prepared one suspension with osteogenic differentiated cells and one suspension with undifferentiated cells, as control. Indeed, four mice were used to test the capability of the cells to differentiate in vivo.

Mice were sacrificed and dissected at 4 weeks after cell transplantation.

In the second trial, the number of cells suspended were raised to 2×10^5 cells as well as the volume of the solution, that was raised to 200 μ l. For each group were prepared the same suspensions, and four mice were used also for this test.

Mice were sacrificed and dissected at 8 weeks after cell transplantation.

2.22 Statistical analysis

All assays were performed in triplicate. The data were reported as means \pm SD and compared using the appropriate version of Student’s unpaired t-test or One way Anova analysis of variance and post Tukey’s multiple comparison test. $p < 0.05$ was considered statistically significant.

Results

3.1 Inflamed dental tissue-derived MSCs

The DPSCs and GMSCs were isolated from 49 patients. The subjects were divided into two major groups: 1) periodontally-compromised group (P, n=37, test group) and 2) healthy group (H, n=12, control group). For each patient pulpal and gingival tissues were extracted. Nine of the total samples (n=5 test group; n=4 control group) were unsuccessfully processed, because of a high grade of bacterial contamination. For all 40 samples, after enzymatic digestion a cell suspension was generated. The first plastic adherent cells were detected from all cultures within seven or ten days of preparation. Initially primary cells from healthy tissue grew faster than those from test group. The cell cultures (p0) appeared heterogeneous in shape and size, and the cells showed the ability to grow out from tissue not totally digested and to form a clone-like growth (Fig.2 a-b, e-f). Generally, in culture progress, gingival cells reached confluence at day 15 (12-18 days) and pulpal cells at day 20 (14-26). All the primary cells showed typical fibroblast-like morphology and they were homogeneous in shape and size (Fig.2 c-d, g-h).

After they reached confluence, the cells were harvested and sub-cultured. From culture p1, a modest change in growth behaviour was observed: although the MTT assay revealed no difference ($p < 0.05$) in the growth rate, the P-DPSCs and P-GMSCs proliferated faster than healthy control cells. The doubling time (DT) was established at 34.37 ± 5 hrs vs. 28.83 ± 2 hrs for H-DPSCs vs. P-DPSCs, respectively; and at 29.13 ± 4 hrs vs. 26.22 ± 8 hrs, for H-GMSCs vs. P-GMSCs, respectively. The cell cycle analysis assigned a proliferation index (P.I.) G2M+S of 7.7% vs. 3.43%, respectively for P-DPSCs vs. H-DPSCs and a P.I. of 23.85% vs. 10.2%, respectively for P-GMSCs vs. H-GMSCs. The difference in P.I. H-DPSCs vs. P-DPSCs and H-GMSCs vs. P-GMSCs was statistically significant (Fig.3).

3.2 Test and control dental pulp and gingival cell express putative mesenchymal stem cells markers; they were negative for hematopoietic differentiation clusters and showed a stem gene profile

The isolated cells did not display any hematopoietic surface markers (CD34 and CD45) and HLA-DR. A slight increment was detected in the expression level of CD34 in test group, but was not statistically significant ($p > 0.005$) (Fig.4). We analyzed the expression of putative mesenchymal surface stem cell markers

Stro-1, CD146, CD29 and SSEA4 by flow cytometry, compared to BM-MSCs (positive control, not showed) (Fig.5). In all samples, CD29 remained highly positive (about 100%). A higher Stro-1+/CD146+/SSEA-4+ cell population was detected in P-DPSCs and P-GMSCs than in the respective healthy controls ($p < 0.05$) (Tab.3).

We compared the stem molecular expression pattern in the H-DPSCs and H-GMSCs, P-DPSCs and P-GMSCs. Expression analysis showed significant differences in ABCG2, CD105 and in OCT4 and SOX-2 mRNA levels in GMSCs vs. DPMSCs, and in P-GMSCs vs. H-GMSCs. Generally, the MSC markers were consistently more highly expressed in dental MSCs than in BM-MSCs (Fig.5c).

3.3 The pro-inflammatory cytokine cocktail could facilitate dental pulp and gingival mesenchymal stem cells expansion in vitro

We investigated the effect of pro-inflammatory cytokines IL-1 β and TNF- α .

After 72 hours of treatment, no cytotoxic effect on cells was detected and by contrast we found increased proliferation. In this connection, MTT analysis showed an increment in the percentage of vital cells and a decrease in DT was detected in H-DPSCs and H-GMSCs treated with IL-1 β and TNF- α , miming a P-DPSC and P-GMSC proliferation curve (Fig.6 a-b).

3.4 Inflammation and stem cell gene profile correlation

To investigate whether the inflammation environment affects stem gene profile, a real-time PCR analysis was performed to compare H-GMSCs and H-DPSCs after 20ng/ml IL-1 β and 40ng/ml TNF- α up to 72 hours treatment versus no treated H-GMSCs and H-DPSCs. In figure 6c and 6d, the histograms represent the mRNA levels expressed as a fold change (FC). In cytokine-treated H-GMSCs and H-DPSCs all MSC markers showed an increase of about 1.5 FC respect to H-GMSCs and H-DPSCs.

We found a statistically significant increase of about 1.52 and 1.37 FC in ABCG2, 1.19 and 1.6 FC in CD105, 1.18 and 1.77 FC in NANOG, 1.77 and 1.14 FC in OCT4, 2.89 and 1.83 FC in SOX-2, respectively in H-DPSCs plus cytokines vs. H-DPSCs and H-GMSCs plus cytokines vs. H-DPSCs ($p < 0.05$).

3.5 Bone in vitro formation: Inflammation – cytoskeleton modulation – osteogenesis

To evaluate the effect of the inflammatory condition on osteogenic differentiation potential in vitro, H-DPSCs and H-GMSCs treated with IL-1 β and TNF- α for 72 hours were cultivated in the ODM and compared to P-DPSCs and P-GMSCs not cytokine-treated. After 21 days of differentiation culture procedure, phenotype and gene analysis were performed. As shown in figure 7a and 7b the alizarin red-positive area indicated a higher amount of calcium deposits in treated H-DPSCs, H-GMSCs and in P-DPSCs, P-GMSC compared to their healthy controls.

3.6 Inflammation increases the expression of differentiation-associated genes

A computational STRING investigation brought to our attention an interaction between inflammation

and cytoskeleton remodeling (fig.7c). To investigate whether the increase in osteogenic potential was correlated with both alteration of inflammation-related gene expression and actin modulation, we examined several HSP and ADF genes. After ten days of osteoblastic differentiation culture the mRNA levels of runx2, vcl, cfn-1 and pfn-1, hsp90, hspA9 and txn-1 expression were observed.

Confirming the higher osteogenesis in inflamed conditions, mRNA level increments of runx2 (specific osteoblastic nuclear factor) in P-DPMSCs, P-GMSCs and cytokine-treated dental MSCs were found. At the same time, we detected a decrease in cofilin-1 and profilin-1 expression and an increase in vinculin-1, hsp90, hspA9 and txn-1 in P-DPMSCs, P-GMSCs and in treated dental MSCs (fig.7d-e).

3.7 Scaffolds preparation and CCK assay

A homogeneous ternary solution of L-poly(lactic acid) (PLLA) was used to create porous scaffolds via TIPS technique. All the produced scaffolds were analysed by mean of the SEM. From the sample holder-like scaffold were made PLLA disks, with a diameter of 6 mm and a thickness of 2 mm. The surface analysis of the samples allowed to define the surface area available for each scaffold, which was approximately equal to 10 cm². In addition, before the cell seeding, all the scaffolds were sterilized, as described before, and coated with collagen type I (200µm/ml).

The first scaffolds prepared (a and b) presented bigger micropores than scaffolds c, in detail: a) 150 µm, b) 50/70 µm, c) 5/20 µm.

The decision to create scaffold with smaller micropores was taken after the CCK assay of the scaffolds a and b. Cell culture tests carried out on these supports showed a quick decrease of the number of viable P-GMSCs cells seeded on the surface of the scaffolds during the examined culture period (10 days) (fig. 8).

For these reason, new scaffolds with smaller pores, (5/20 µm), were produced.

The new scaffolds presented smaller micropores and high degree of interconnection (fig 9 and fig 10). Moreover, due to the results of the CCK assay, it was decided to seed 75000 cells for scaffold; so a cell suspension with 1x10⁵ P-GMSCs for microliter density was seeded on every scaffolds. All experiments were performed in triplicate

3.8 2D Alamar Blue assay

The observation of the P-GMSCs growth showed a slow growth, strictly dependent to the cell density in the plates.

For that reason, in order to evaluate the ideal cell concentration to achieve a rapid cell growth on the scaffolds, a 2D Alamar Blue assay was carried out on P-GMSCs cells seeded at different concentrations.

In the fig. 11, it is possible to observe the P-GMSCs cell growth at different times. It was possible to observe how this cell type tends to stretch to make contact with neighbouring cells, at low cellular

density. Moreover, some P-GMSCs assumed a more similar astrocytes-like phenotype, as shown in fig. 12.

The results in fig. 13 showed a faster cell growth when the cell concentration was greater than 7500 cell/cm². These data were essential to establish the ideal cell concentration for the successive seeding; additionally, it was defined that the ideal dimension of the flasks was of 25 cm².

3.9 3D Alamar Blue assay

The Alamar Blue assay, as described before, was used to evaluate the cell growth (fig. 14). The data showed the continuous cell growth in the studied period (120h), in which there was a doubling of the cells number present in the scaffold c. Comparing this curve with the previous one, related to the scaffold a and b, it is evident the difference in terms of cell growth between the two groups of the scaffolds.

3.10 AO/EB vitality assay

The observation of the scaffolds c through fluorescence microscopy at 72h confirmed a high level of cell viability (fig. 15). Indeed the red spot, related to non-viable cells, are few and circumscribed to few areas of the examined scaffolds.

3.11 DAPI assay

By nuclear staining and fluorescence microscopy, it was possible to observe the P-GMSCs distribution on the scaffolds c.

The acquired images, taken in different regions of the seeded scaffolds, showed that the cells are distributed homogeneously over the entire scaffold's surface (fig. 16).

3.12 In vivo studies

In the first animal study group was not observed bone formation at 4 weeks after cells transplantation (fig.17).

So, in the second study group, it was decided to increase the number of cells suspended, the volume of the cells suspension and the period of time before the sacrifice of the animals. Again, in the second animal study group was not observed bone formation at 8 weeks after cells transplantation (fig.18).

In both the animals were not presented any bone formation neither inflamed tissue formation.

CHAPTER 4

Discussion

For decades now extraordinary interest has matured in the field of MSCs because of their differentiation potential, which has led them to be used in TE, RM and cell and gene therapy for clinical applications. The search is ongoing for the best MSC tissue source. The elective tissues for this purpose are bone marrow and adipose tissue, although isolation of these MSCs may be an invasive procedure for patients and donors. In view of this, the possibility of isolating MSCs from discarded tissue is a fascinating idea and MSCs from periodontally-compromised teeth could be a good alternative. Even though it has been shown in the literature that pro-inflammatory cytokines affect MSC properties, the effects of inflammation due to periodontitis and its progression on the characteristics of dental MSCs remain unclear^{47,58,69}.

In the present study, we confirmed the presence of MSCs in human dental pulp and gingival tissue harvested from periodontally-compromised teeth and for the first time, to the best of our knowledge, at the same time we compared simultaneously the stem features to DPSCs and the GMSCs harvested from healthy donors. The cells isolated from all groups showed a typical fibroblast-like shape and proved positive for the principle stem markers (Stro-1, CD46, CD29 and SSEA4) and they did not exhibit surface expression for any hematopoietic marker (CD34 and CD45). Our results suggest that the inflamed condition related to the periodontal status of the patients has no effect on dental MSC viability, whereas it seems to improve the growth ability and stem gene profile of DPSCs and GMSCs. This view is supported by pro-inflammatory cytokine precondition experiments that demonstrated that H-DPSCs and H-GMSCs are able to mimic P-DPSCs and P-GMSCs, displaying similar proliferation curves and gene expressions when treated with IL-1 β and TNF- α .

P-DPSCs and P-GMSCs show a clear higher expression of the cardinal stem nuclear markers (NANOG, OCT4 and SOX-2) and ABCG2 (superficial marker) compared to both H-DPSCs and H-GMSCs and the internal positive control (BM-MSCs). Moreover, our data about H-DPSCs and H-GMSCs under pro-inflammatory conditions in vitro show that osteoblastic differentiation capacity is not only well preserved but also is significantly improved compared to not stimulated and is almost equal to the MSCs of the test group. This finding was confirmed by a more highly calcified extracellular matrix formation and a higher expression of runx2, a bone-specific transcription factor, in

the cytokine-treated H-DPSCs and H-GMSCs as well as in the P-DPSCS and P-GMSCs⁷⁰⁻⁷². Furthermore, we found that in the inflamed environment the expression levels of profilin-1 and cofilin-1 decreased, whereas vinculin and hsp90, txn-1 and hspA9 permit stabilization of actin filaments. It has already been shown that in inflammatory environments several mediators activate a set of biological processes such as cell survival, proliferation and cell differentiation in MSCs⁷³⁻⁷⁶. During lineage specific differentiation, human stromal stem cells exhibit significant changes in morphology and actin cytoskeleton organization⁷⁷⁻⁸². ADFs bind to actin monomers and filaments, causing depolymerization of actin filaments and thus preventing their reassembly and decreasing osteoblastic differentiation⁸²⁻⁸⁶. Osteoblastic cytoskeleton reconstruction depends on the regulation of the actin polymerization status carried out by ADFs, including cofilin, profilin and vinculin⁸⁷⁻⁸⁹.

In recent years, one of the most studied materials has been the PLLA, which, in the present study, was used to develop scaffold by mean of the TIPS technique. The scaffolds were prepared according to a previously published technique by Pavia et al^{64,68}, allowing the formation of foams with an ordered multilevel structure and average micropores size ranging from 150 μm to 5/20 μm .

After the first in vitro study on scaffold a (150 μm) and scaffold b (50-70 μm), we observed a quick decrease of the number of viable P-GMSCs cells seeded on the surface of the scaffolds during the examined 10 days of culture period. For these reason, a different protocol was adopted to devolp a new scaffolda smaller micropores (5/20 μm) and high degree of interconnection.

Once we have defined the size of the micropores of the scaffold by mean of the 2D Alamar Blue assay, we evaluate the ideal cell concentration to achieve a rapid cell growth on the scaffolds.

In the second in vivo study on scaffold c, P-GMSCs showed the capability to grow on PLLA scaffolds. It was observed that P-GMSCs tend to assume an astrocytes-like phenotype and showed a faster cell growth when the cell concentration was greater the 7500 cell/cm². These data were essential to establish the ideal cell concentration for the successive seeding.

Due to the 3D Alamar Blue assay and the AO/EB vitality assay, the P-GMSCs have shown a good proliferation rate, a high level of cell viability and low cells mortality.

Furthermore, due to the DAPI assay, it was possible to observe on homogeneous distribution of the P-GMSCs on the scaffolds c.

Indeed, it could be assumed that PLLA scaffolds with 5/20 μm micropores promote the adhesion and the replication of P-GMSCs.

Regarding the in vivo study, in both the animals study groups were not presented any bone formation neither inflamed tissue formation, at 4 or 8 weeks.

Probably these results are related to the unstable carrier chose for the implantation of the cells; the skin absorption of the suspension was to fast, not giving to the cells the time needed to induce bone formation in vivo.

New in vivo studies are ongoing: cells suspensions of H-DPSCs, P-DPSCs, H-GMSCs or P-GMSCs were seeded on new scaffolds, with the same characteristics of scaffold c. After one week of in vitro osteogenic differentiation, the scaffolds were transplanted subcutaneously on the dorsal surface of 6-week-old immunodeficient nude mouse (NU/NU).

In conclusion, our results confirm that the chronic inflammatory microenvironment existing in periodontitis does not negatively affect the number of P-DPSCs and P-GMSCs and their stem cell marker profile. Pro-inflammatory cytokines permit a higher osteogenic differentiation potential, controlling the fate of MSCs through several regulatory mechanisms involving remodeling of cytoskeleton and stress response processes. Our data need further confirmation using enriched P-DPSCs and P-GMSCs engineered scaffolds with the same set of experiments as presented in this study (data in progress). The first results about the growth and differentiation potential of seeded cells “in and from” the inflammatory environment are very promising. In our experience, P-DPSCs and P-GMSCs appear to be a valid autologous MSC source. In addition, they are promising for in vivo applications in diseases with persistent inflammatory environment that generally harms the features and hinders the success of cell transplantation. From a clinical point of view, our findings confirm the feasibility of tissue engineering and regenerative medicine applications in vivo.

CHAPTER 5

Tables and Figures

5.1 Tables

PRIMARY ANTIBODY/ LOCALIZATION MARKER	CODE NUMBER	DILUTION	INCUBATION
Stro-1, surface	Thermo Fisher Sc, 39-8401	1:100	Overnight (o/n), room temperature (r.t.)
CD 146, surface	Milteny Biotec, 130-092-851	1:50	30 min, room
CD 29, surface	Milteny Biotec, 130-101-258	1:50	30 min, room
SSEA4, surface	Milteny Biotec, 130-98-371	1:100	30 min, room
CD-34, surface	Santa Cruz, sc-19621	1:50	o/n , r.t.
CD-45, surface	Santa Cruz, sc-28369	1:50	o/n , r.t.
HLA-DR, surface	Santa Cruz , sc-18875	1:50	o/n , r.t.
SECONDARY ANTIBODY	CODE NUMBER	DILUTION	INCUBATION
AlexaFluor 488	Life Technologies, Z25402	1:50	20 min, r.t.
AlexaFluor 594	Life Technologies, Z25007	1:50	20 min, r.t.

Table 1: Human anti-monoclonal antibodies list used in flow cytometry analysis for detection of MSC markers.

GENE	PRIMER SEQUENCE	CODE NUMBER
ABCG2		QT00073206
CD105		QT0001335
THY-1		QT00023569
CD73		QT00027279
NANOG		QT01844808
OCT4		QT00210840
SOX2	<i>F:5'- GGAGACGGAGCTGAAGCCGC-3'</i> <i>R:5'GACGCGGTCCGGGCTTGTTTT-3'</i>	MWG
HSPA9 (mortalin)	<i>F:5'-TACAGCAGATGGTGAGCGAC-3'</i> <i>R:5'-TGCTGTGTGCCCAAGTAAT-3'</i>	MWG
TXN-1 (thioredoxin-1)	<i>F:5'- GTGAAGTCAAATGCACGCCA-3'</i> <i>R:5'-GCAGATGGCAACTGGTTATGT-3'</i>	MWG
HSP90AA1	<i>F:5'-GTGAAGTCAAATGCACGCCA-3'</i> <i>R:5'-GCAGATGGCAACTGGTTATGT-3'</i>	MWG

Table 2: The primer sequence list used for the amplification of MSC cDNA.

MSCs	MESENCHYMAL STEM CELL MARKERS			
	STRO-1	CD146	CD29	SSEA4
H-DPSCs	12.30 ± 2.32 %	18.95 ± 1.79 %	99.07 ± 0.5 %	18.31 ± 1.06 %
P-DPSCs	31.32 ± 3.32 %	37.80 ± 4.79 %	97.26 ± 2.38 %	27.33 ± 2.71 %
H-GMSCs	10.61 ± 1.37 %	73.34 ± 5.43 %	96.64 ± 5.08 %	17.72 ± 1.97 %
P-GMSCs	20.46 ± 2.18 %	86.54 ± 3.76 %	96.74 ± 3.68 %	31.56 ± 2.54 %
BM-MSCs	6.25 ± 2.2 %	44.89 ± 5.54 %	97.21 ± 0.89%	5.1 ± 1.53 %

Tab. 3 The MSCs marker level expressions in healthy and periodontally-affected DPSCs or GMSCs. Standard deviations (±).

5.2 Figures

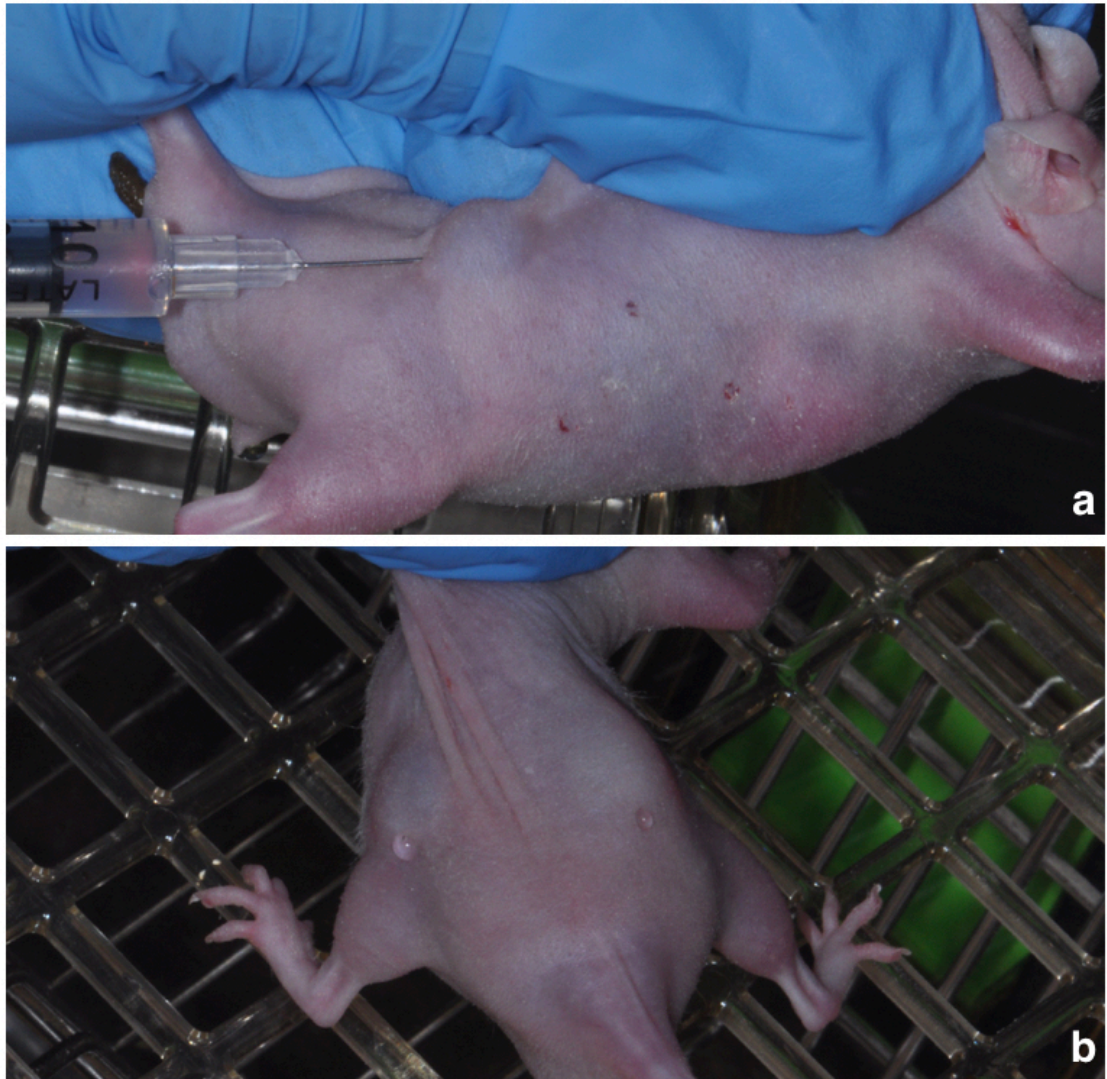


Fig. 1 Inoculation of the cells suspension subcutaneously on the dorsal surface of NU/NU mouse

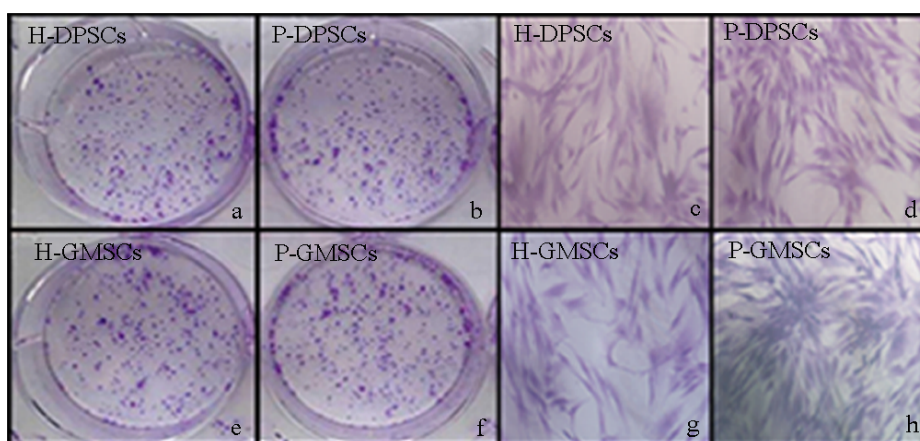


Fig. 2 Colony-forming unit assays and monolayer subculture: Representative image of pulpal or gingival mesenchymal stem cell colonies stained with crystal violet isolated from teeth of one healthy subject and one periodontal-affected patient. Figures a and b, e and f show the clone-like growth of H-DPSCs and P-DPSCs, respectively. Figures c and d, g and h show the typical fibroblast-like morphology of H-GMSCs and P-GMSCs (40x).

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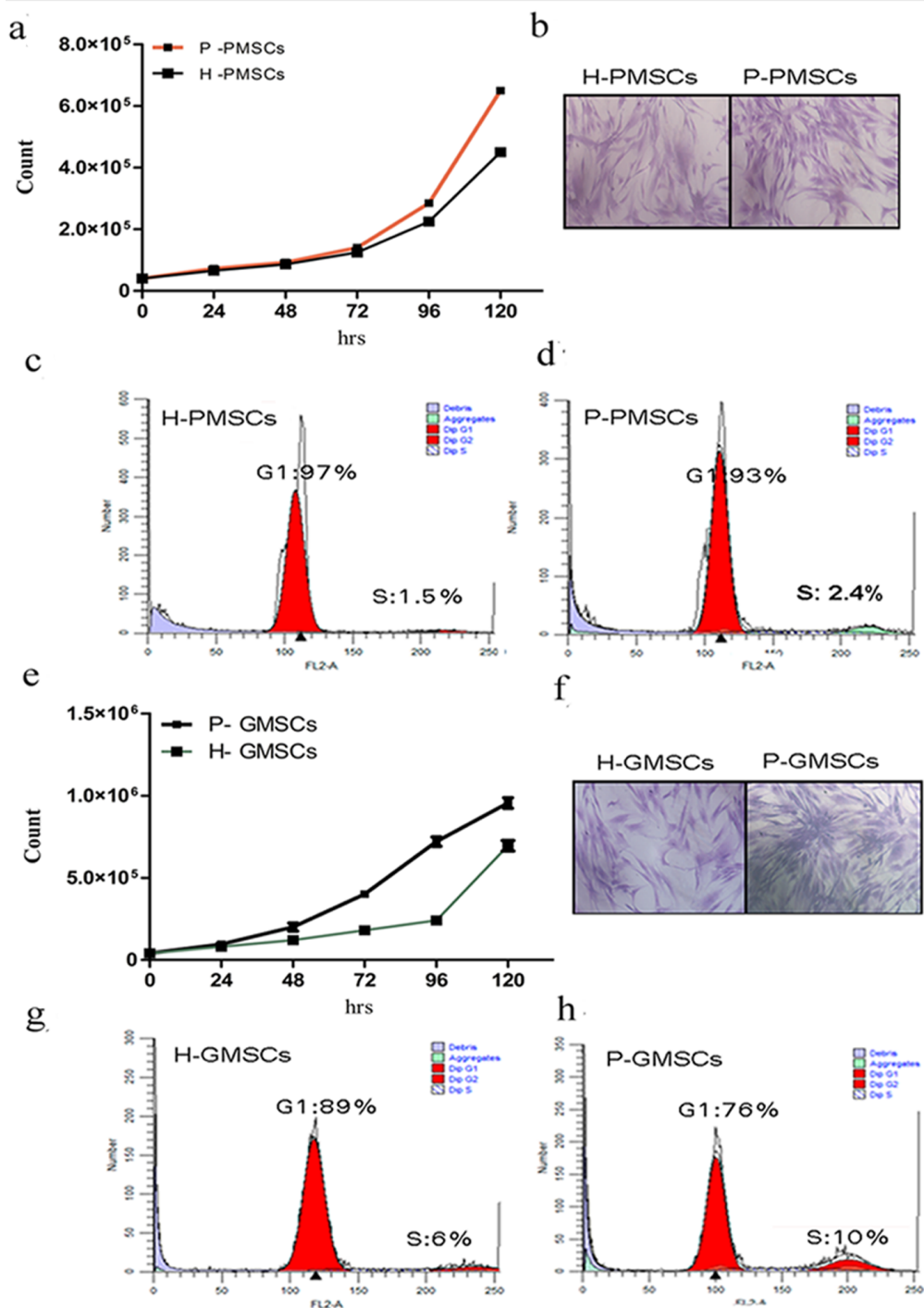


Fig.3 Proliferation curve and cell cycle analysis: In the upper panel: a) Cell growth curve of H-DPSCs and P- DPSCs evaluated with Trypan blue viability assay; b) From the typical fibroblast-like cell shape the higher P- DPSCs cellular density at 72 hrs is evident (40x); (c-d) A representative comparative analysis between cell cycle distribution of H-DPSCs and P-DPSC. In low panel: e) Cell growth curve of H-GMSCs and P-GMSCs with Trypan blue viability assay; f) H-GMSCs and P-GMSCs at 72 hrs; the P-GMSC cell density is higher than that of H-GMSCs (40x); (g-h) A representative comparative analysis of proliferative activity cell cycle distribution of H-GMSCs and P-GMSCs.

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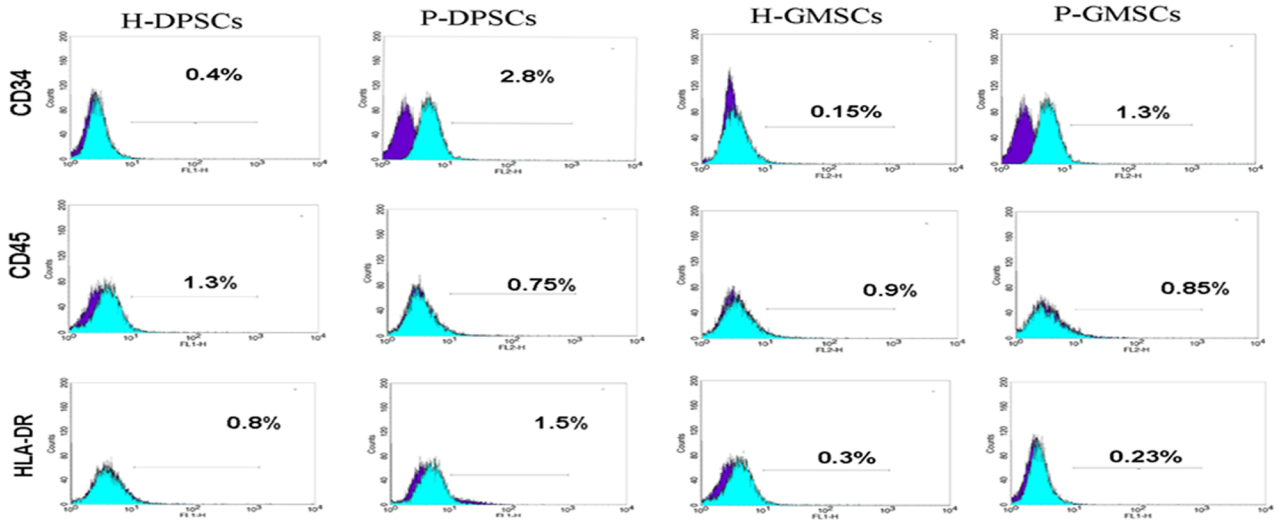


Fig.4 Immuniphenotype flow cytometric assay: Cells are negative for CD34, CD45 and HLA-DR. All fields are representative of one sample. The CD34 increment in a periodontal-affected sample was not statistically significant.

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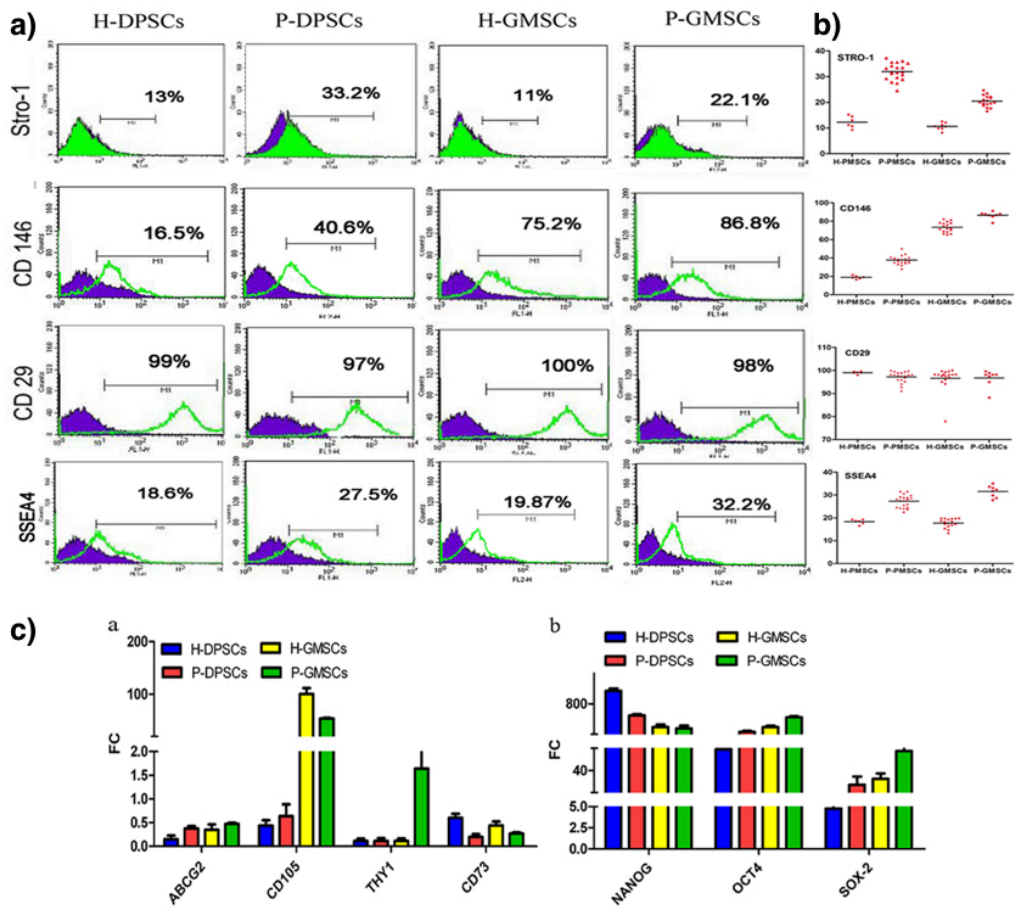


Fig.5 Stem cell feature analysis: a) A representative flow-cytometric analysis of periodontal-affected pulpal or gingival MSCs (P-DPSCs and P-GMSCs) in comparison to healthy controls (H-DPSCs and

H-GMSCs); b) The scatter dot plot graph represents the expression levels of mesenchymal stem cell markers (STRO-1; CD146; CD29 and SSEA4); c) the histograms represent a comparative qRT-PCR analysis of nuclear (on the left) and surface (on the right) markers in H-DPSCs, P-DPSCs, H-GMSCs and P-GMSCs. Actin- β was used as the housekeeping gene. FC (fold change). The mRNA expression of all analyzed genes was normalized against BM-MSCs (positive control).

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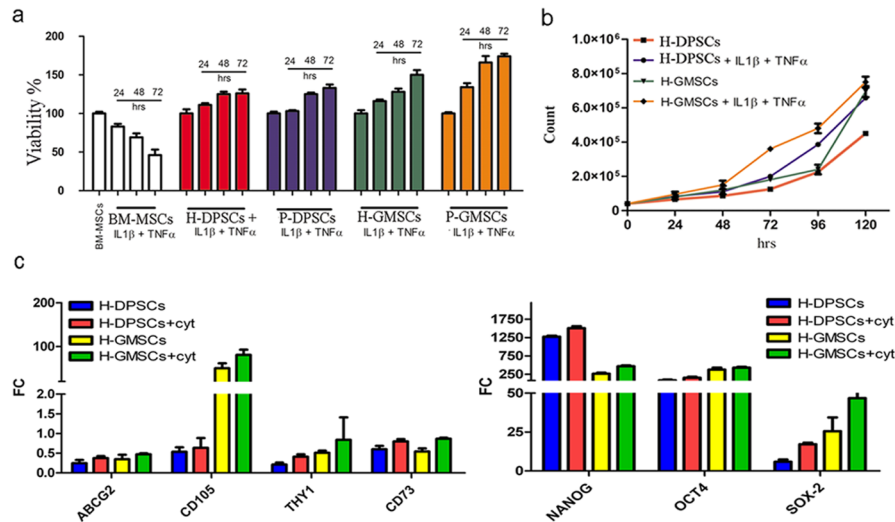


Fig.6 Two cytokines promote H-GMSC and H-DPSC expansion. a) Cytotoxicity assay: H-DPSCs, H-GMSCs without and after cytokine treatment; b) Cell growth curve of H-DPSCs and P-DPSCs without and after cytokine treatment evaluated with Trypan blue viability assay; c) Comparative analysis of nuclear (on left) and surface marker expression (on right) in H-DPSCs and H-GMSCs with or without cytokine treatment (20ng/ml IL-1 β and 40ng/ml TNF- α for 72 hrs).

BM-MSCs: positive control; β -actin: normalized gene.

Mean values \pm SD of all samples studied are reported. Error bars are based on 3 independent experiments.

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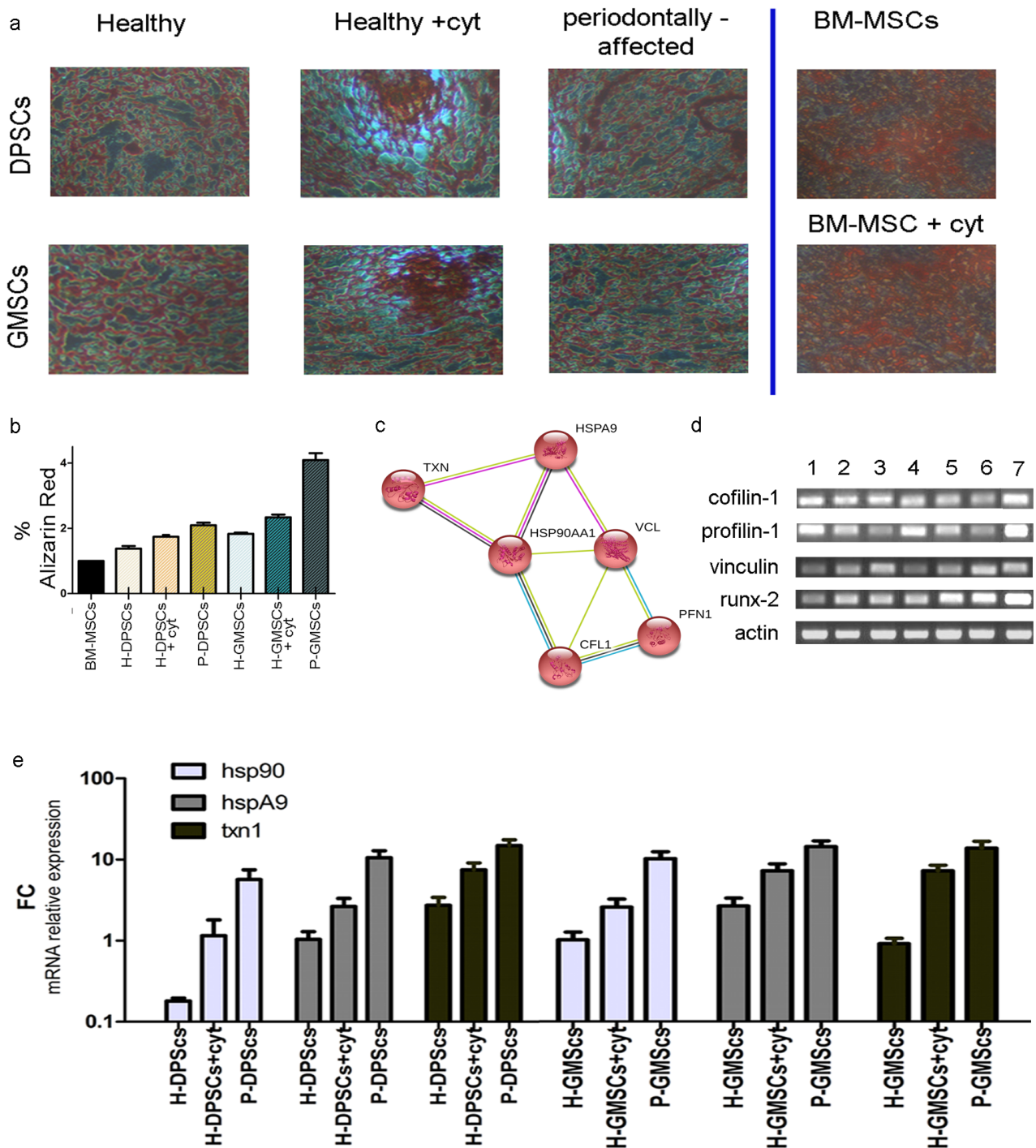


Fig.7 Bone in vitro formation: Inflammation – cytoskeleton modulation -osteogenesis: a) A representative image of Alizarin Red assay stained calcium deposits after 21 days of osteogenic differentiation of cultured H-DPSCs, H-GMSCs with or without cytokine treatment, P-DPSCs, P-GMSCs and BM-MSCs (control); b) the bar graph represents the quantitative analysis of the alizarin positive area performed with ImageJ software; c) the graph represents the interaction between anti-inflammatory and cytoskeleton-regulating proteins performed on <http://string-db.org/>; d) the gel lines represent the semi-quantitative PCR analysis for runx- 2, vinculin, profilin-1 and cofilin-1 (1: H-DPSCs; 2:H-DPSCs + cyt; 3: P-DPSCs; 4: H-GMSCs; 5: H-GMSCs + cyt; 6: P-GMSCs; 7: Positive control. cyt:20ng/ml IL1 β + 40ng/ml TNF- α); e) the bar graph represents hsp90, hspA9 and txn1 real-time PCR analysis normalized to BM-MSCs control; (cyt: 20ng/ml IL-1 β + 40ng/ml TNF- α). FC: fold change.

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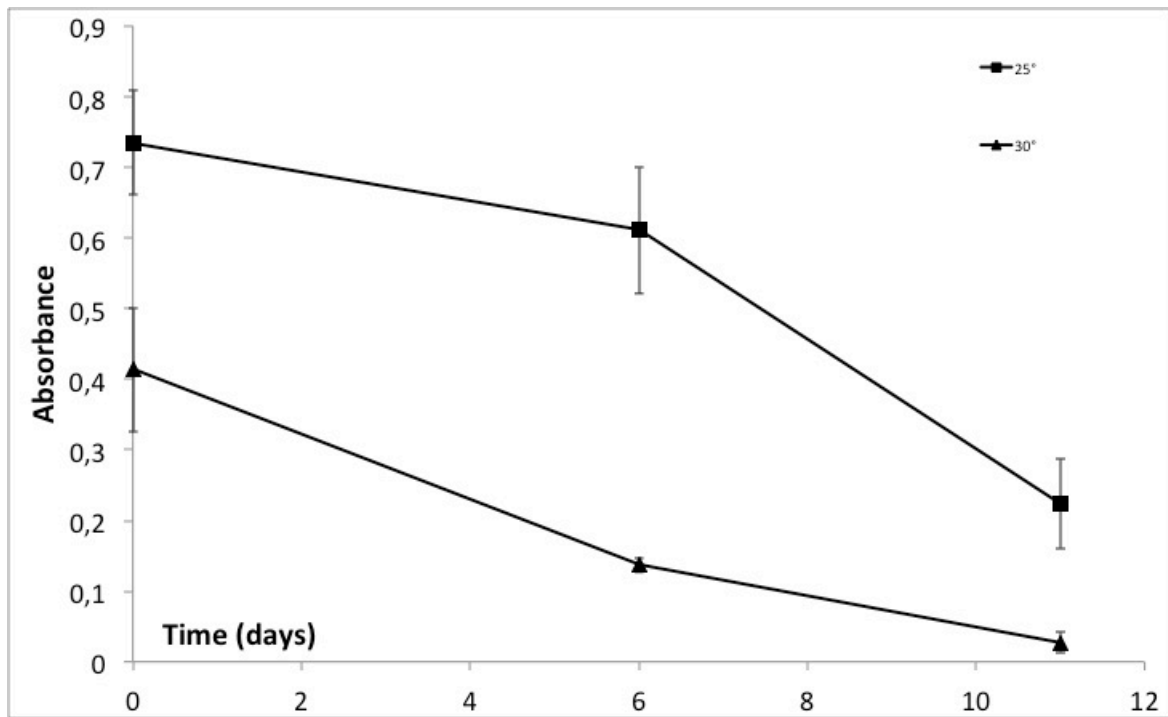


Fig. 8 CCK assay: Cell culture tests carried out on these supports showed a quick decrease of the number of viable P-GMSCs cells seeded on the surface of the scaffolds a and c during the examined culture period.

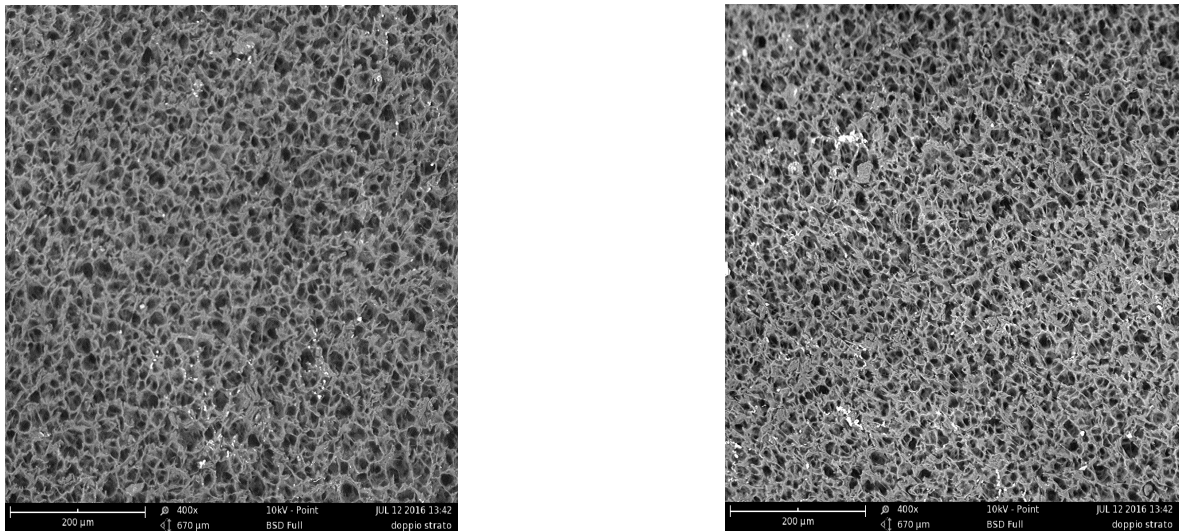


Fig. 9 SEM images of new scaffolds with smaller pores, (5/20 μm), 400x magnification

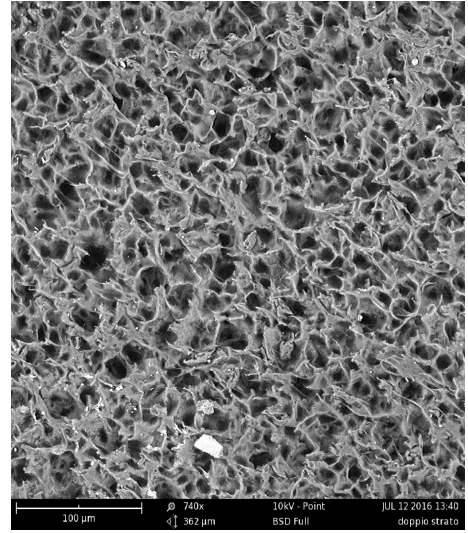
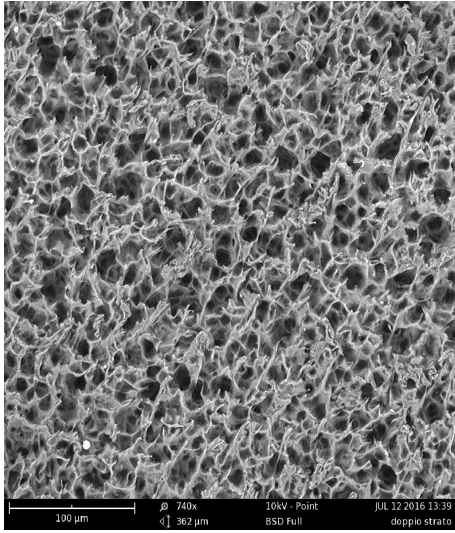


Fig. 10 SEM images of new scaffolds with smaller pores, (5/20 µm), 750x magnification

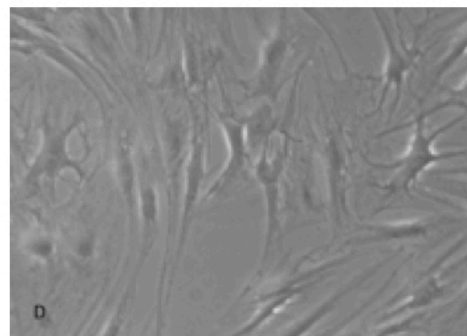
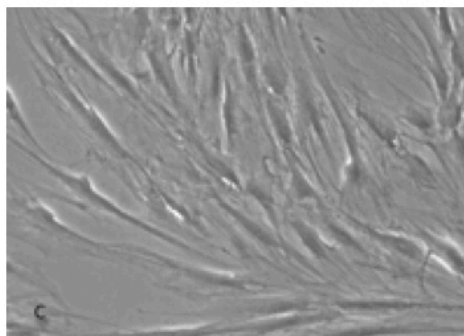
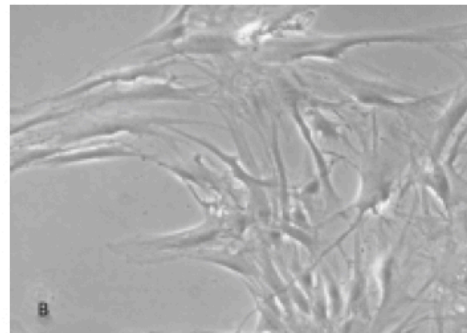
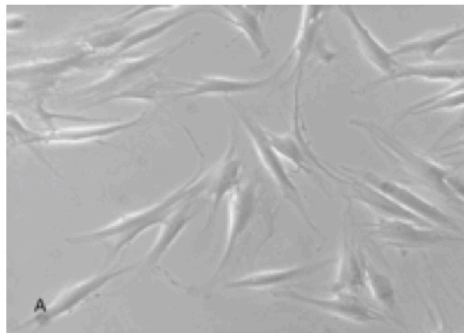


Fig. 11 P-GMSCs cell growth at different times. a) day 1; b) day 3; c) day 6; d) day 7.

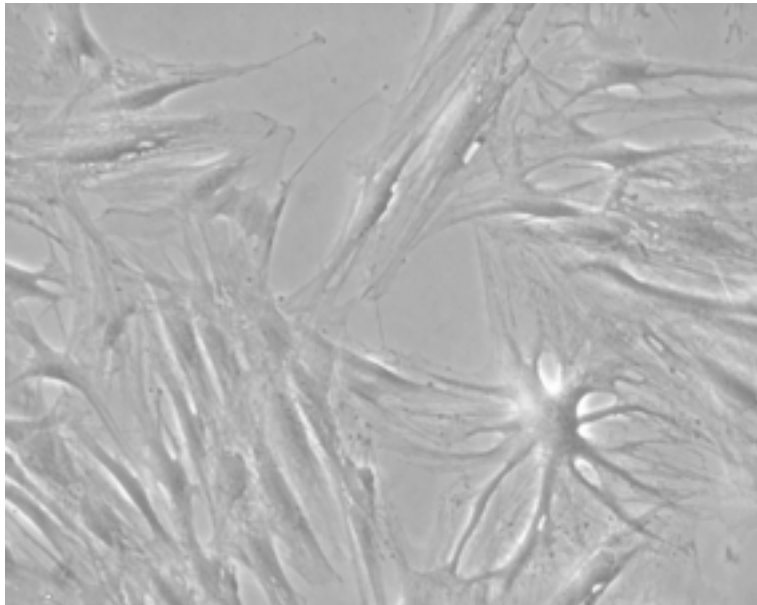


Fig. 12 P-GMSCs cell growth: similar astrocytes-like phenotype, day 6

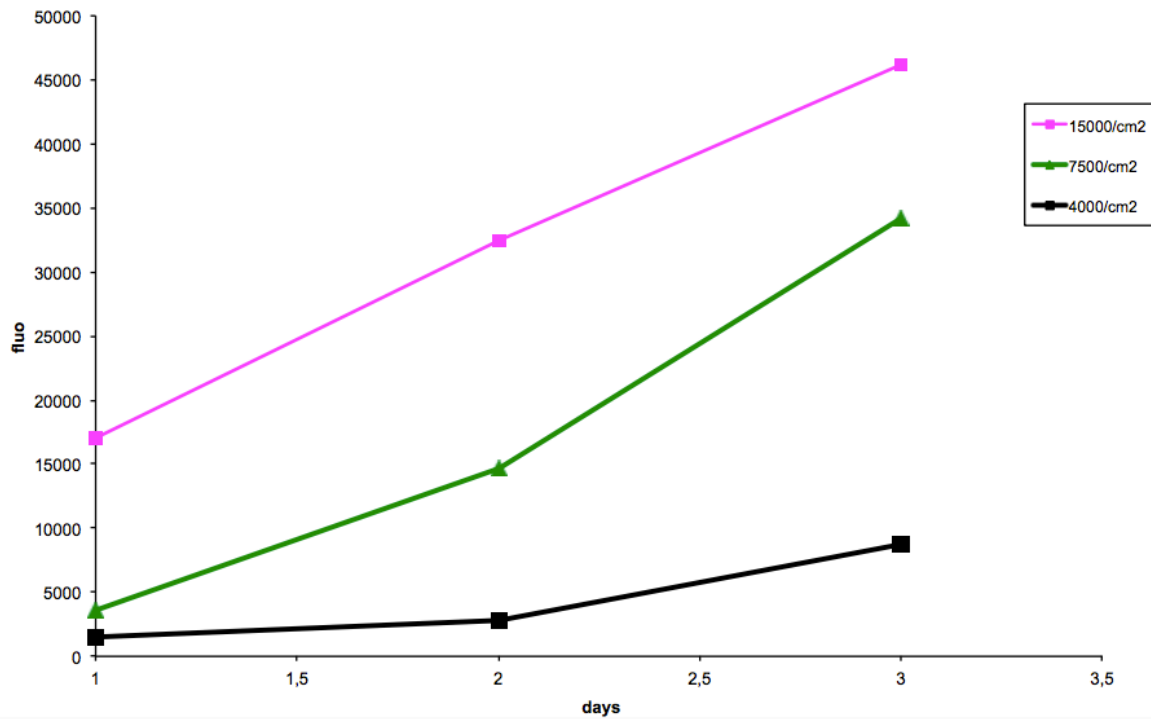


Fig. 13 P-GMSCs growth curve in 2D, plated at different cell concentrations, assessed by Alamar Blue assay

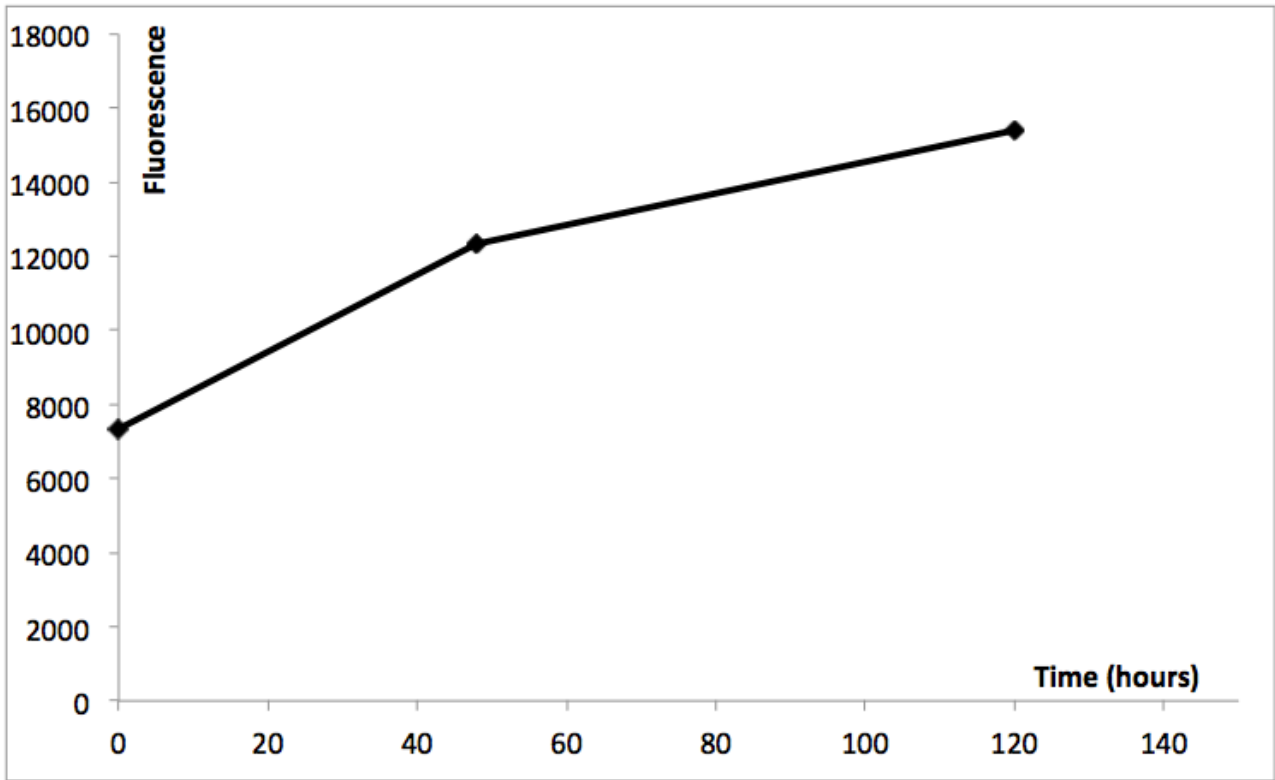


Fig 14 P-GMSCs Growth curve, on scaffold c, assessed by Alamar Blue assay

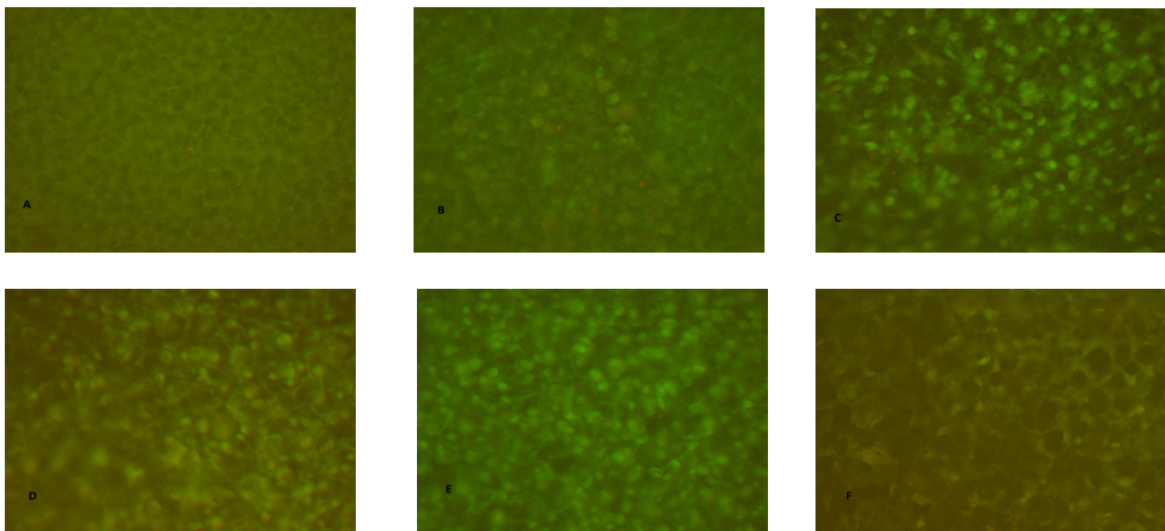


Fig. 15 AO/EB vitality assay of P-GMSCS on scaffold c

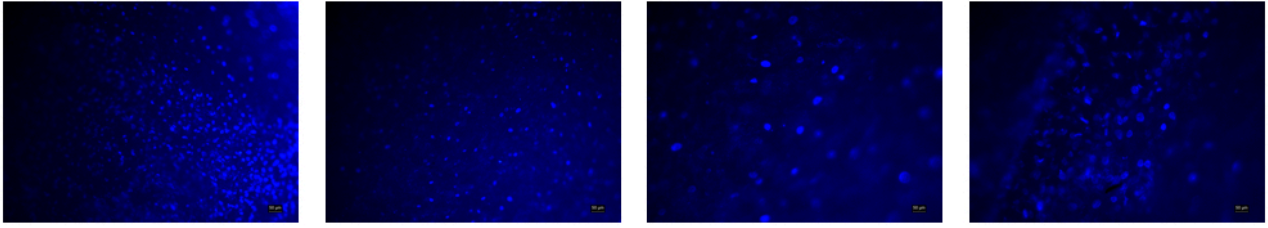


Fig. 16 DAPI assay of the P-GMSCs seeded on the scaffold c



Fig. 17 In vivo study: in the picture the dorsal surface of one mouse of the first animal study group, no bone formation was observed

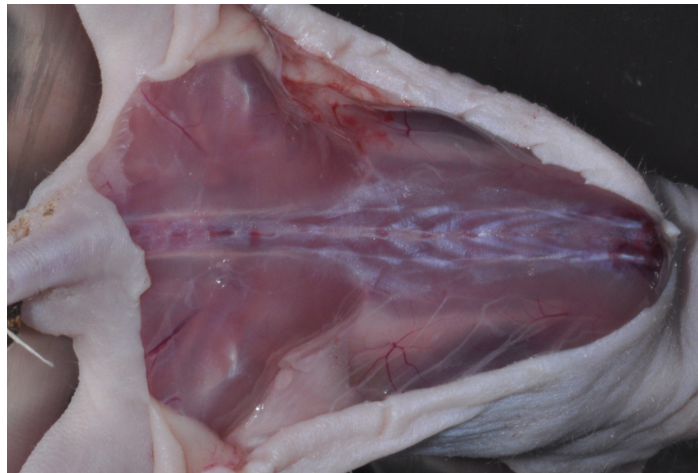


Fig. 18 In vivo study: in the picture the dorsal surface of one mouse of the second animal study group, no bone formation was observed

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Scientific Products (bound)

Publications discussed in this thesis:

"In vitro investigation on stem cells isolated from dental pulp and gingival tissues from periodontally compromised teeth."
R. Mauceri, L. Tomasello, C. Giordano, G. Campisi, G. Pizzo. "I & J. Quintessenza Internazionale & Jomi", numero 4/2015 pagina 56;

"Mesenchymal stem cells derived from inflamed dental pulp and gingival tissue: a potential application for bone formation". L. Tomasello, R. Mauceri, A. Coppola, M. Pitrone, G. Pizzo, G. Campisi, G. Pizzolanti, C. Giordano. Stem Cells Translational Medicine (Submitted)

Publications not included in this thesis:

2014

"A simple protocol for medical-surgical tooth extractions in patients treated with bisphosphonates: our experience." ME Licata, A. Albanese, R. Mauceri, G. Giannatempo, L. Lo Russo, L. Lo Muzio. Minerva Stomatologica – Vol. 63 Suppl. 1 al N.4 (Aprile 2014), pagina 495;

"Segmental resection for the excision of two multicystic ameloblastoma". G. Capocasale, D. Perrone, R. Mauceri, B. Polizzi, L. Laino. Annali di Stomatologia No. 3 Vol. V - No. 2 - April/June 2014 – Quarterly, pagine 15-16;

"Evidence of field cancerization of oral squamous cell carcinoma: a case report". V. Panzarella, R. Mauceri, M. Dioguardi, G. Troiano, O. Di Fede. Annali di Stomatologia No. 3 Vol. V - No. 2 - April/June 2014 – Quarterly, pagina 34;

2015

"Paresthesia of the lip caused by a large osteoma of the mandible treated with a conservative approach: a case report." G. Giannatempo, G. Capocasale, N. Termine, R. Mauceri, L. Lo Russo, M. Giuliani. Minerva Stomatologica – Vol. 64 Suppl. I al N.2 (Aprile 2015), pagina 171;

"The surgical treatment of mandibular peripheral calcifying epithelial odontogenic tumour (pindborg tumor) with Er,Cr:YSGG laser: a case report." M. E. Licata, A. Albanese, G. Giannatempo, M. Dioguardi, R. Mauceri, G. Campisi. Minerva Stomatologica – Vol. 64 Suppl. I al N.2 (Aprile 2015), pagina 173.

"Painful oral aphthous-like lesions in patient with kidney cancer after target therapy and bisphosphonate administration: a case report of adverse drug reaction." R. Mauceri, O. Di Fede, D. Perrone, G. Campisi, L. Laino. Minerva Stomatologica – Vol. 64 Suppl. I al N.2 (Aprile 2015), pagine 176-177;

"Triple simultaneous oral squamous cell carcinoma in a heavy smoker patient: a case report." Mauceri R., Panzarella V., Giuliani M., Lo Muzio L., Di Fede O. Annali di Stomatologia No. 3 Vol. VI Suppl. I - April/June 2015 – Quarterly, pagina 63 -

"Optical coherence tomography as a simple and non invasive tool for the diagnosis of oral disease: a case report." Capocasale G, Mauceri R, Troiano G, Lo Muzio L, Campisi G. Annali di Stomatologia No. 3 Vol. VI Suppl. I - April/June 2015 – Quarterly, pagina 52

"Use of porcine collagen matrix (Mucograft®) to promote the wound healing in the oral cavity". L. Laino, M. Giuliani, R. Mauceri, F. Giancola, G. Troiano. Annali di Stomatologia No. 3 Vol. VI Suppl. I - April/June 2015 – Quarterly, pagine 55-56

2016

“Dual localization of oral Kaposi’s sarcoma in HIV-negative patient: a rare case report”. G. Capocasale, R. Mauceri, De Lillo A, L. Lo Russo, F. Giancola, O. Di Fede. *Minerva Stomatologica* – volume 65 . SUPPL.1.No.3. JUNE 2016, pagine 195-196

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