Synthesis and characterisation of functionalized borosilicate nanoparticles for boron neutron capture therapy applications

S. Grandi · A. Spinella · C. Tomasi ·

G. Bruni · M. Fagnoni · D. Merli · P. Mustarelli ·

G. F. Guidetti · C. Achilli · C. Balduini

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Abstract Boron Neutron Capture Therapy (BNCT) is a promising therapy for the cure of diffuse tumors. The successful clinical application of BNCT requires finding new boron-based compounds suitable for an efficient ¹⁰B delivery to the cancerous tissues. The purpose of this work is to synthesize borosilicate nanoparticles by a sol-gel recipe, and to functionalize them with folic acid in order to promote their capture by the tumor cells. Whereas sol-gel is a promising technique for the synthesis of nanoparticles, in case of borosilicate systems this approach is affected by significant boron loss during preparation. Here we show that functionalization of borosilicate nanoparticles with folic acid can reduce the boron loss. Moreover, preliminary biocompatibility tests indicate that functionalization strongly changes the reactivity of NPs towards blood cells, so favouring the potential use of these materials for clinical applications.

S. Grandi (⊠) · G. Bruni · M. Fagnoni · D. Merli · P. Mustarelli

Department of Chemistry, University of Pavia, V.le Taramelli 12, 27100 Pavia, Italy e-mail: rondine68cub@yahoo.it

A. Spinella CGA, University of Palermo, 14, Via F. Marini, 90128, Palermo, Italy

C. Tomasi I.E.N.I. C.N.R. Department of Pavia, Viale Taramelli 16, 27100 Pavia, Italy

G. F. Guidetti · C. Achilli · C. Balduini Laboratory of Biochemistry, Department of Biology and Biotechnology, University of Pavia, Via Bassi 21, 27100 Pavia, Italy



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1 Introduction

Boron neutron capture therapy (BNCT) can potentially destroy cancer cells in a selective way so minimizing negative effects on healthy tissues. This treatment is based on the selective accumulation into the malignant cells of $^{10}\text{B}\text{-containing}$ compounds administrated by intravenous infusion. Subsequent thermal neutron irradiation promotes ^{10}B decay to one ^{4}He (α particle) and one ^{7}Li atom with a cytotoxic effect that can destroy the tumor cell [1]. To date, medical trials of BNCT had been carried out principally with boronophenylalanine (BPA) that showed a good selectivity to malignant cells. On the other hand, BPA contains only the 5.1 % wt. of boron.

Many classes of nanomaterials are under investigation as possible boron-carriers in alternative to BPA [2, 3]. Functionalization with folic acid improves their uptake in tumor cell lines [4, 5, 6], probably due to the overexpression of folic acid receptors in many types of cancer cells. An example of boron-enriched nanomaterial are Boron Nitride Nanotubes (BNNTs) functionalized with folic acid, recently studied by Ciofani et al. [6], who reported a good uptake on malignant glioblastoma cells. Unfortunately, an important disadvantage of BNNTs is their availability, as to date the production is expensive and limited to the laboratory scale.

As an alternative, it is possible to employ borosilicate porous glasses obtained by sol-gel method which are biocompatible, bioactive and biological resorbable [7]. However, it is difficult to prepare these particles with a

high boron concentration because of the nature of B-O-Si bond that is highly hydrolysable in presence of water (humidity). Many authors reported significant boron lack in their sol-gel samples. Nogami and Moriya [8] prepared different compositions of SiO₂-B₂O₃ and their study showed that for the sample containing more than 20 mol% B₂O₃ a quarter of B₂O₃ was lost during the gel synthesis. The problem of the of Si-O-B bond formation was analyzed by Irwin et al. [9, 10] by means of ²⁹Si and ¹¹B MAS NMR spectroscopy. They showed that the majority of boron atoms in xerogels was in form of boric acid hydrogen-bonded to the silica network, whereas there was only a small amount of B-O-Si bonds. They concluded that the boron leaching was due both to the presence of water and to the high volatility of the trimethoxyborate reagent. Only a thermal treatment performed at about 500 °C was able to transform the boric acid hydrogen-bonded to the silica matrix into a true borosiloxane network. Later in 2002, Li et al. [11] reported both synthesis and characterization of the ternary system SiO₂-B₂O₃-P₂O₅ with different molar ratio. However, in such a paper the loss of boron was hypothesized but not quantified. Soraru et al. [12, 13] found that SiO₂-B₂O₃ gels made by employing organo-modified silicon alkoxides did retain boron in the xerogels by means of the creation of a high number of borosiloxane bonds. Nonetheless, when the boron content was verified by elemental analysis [13], the loss of boron was still detected (about 20-50 %). A very recent work [14] proposed a particular sol-gel synthesis of borosilicate nanoparticles (100–500 nm) by exothermic phase separation, but the real boron content was not verified. Our very recent study [15] on borosilicate xerogels revealed the same problem, which was partially overcame by employing 3-aminopropyltriethoxysilane (APTES) as a co-precursor. These findings are promising for possible application in BNCT therapy: in fact, pre-functionalization of nanoparticles with -NH₂ groups allows the further functionalization with folic acid and could improve the uptake in tumor cells. In this way the presence of -NH₂ groups would play a dual role: as a boron trapper and a primer.

Aim of this work is the preparation of NPs from 2SiO₂ –B₂O₃ xerogels with a top-down method, and their functionalization with folic acid. Many authors have also reported that different classes of nanomaterials are not completely inert toward biological systems and can exert several toxic effects [16, 17]. Furthermore, nanoparticles can induce negative responses of blood components, including neutrophil activation [18] and platelet aggregation [19, 20]. Therefore, biocompatibility tests on platelets and neutrophils were performed in order to evaluate whether borosilicate NPs, and the corresponding folate-functionalized counterparts, can be suitable for intravenous injection for BNCT.

2 Experimental

2.1 Preparation of 2SiO₂–B₂O₃ xerogel (sample SiB)

10.39 g of trimethylborate (TMB) were dissolved in 30 ml of methanol and 3.6 ml of H_2O , and stirred for 1 h in order to complete the hydrolysis stage, then 15.22 g of tetramethoxysilane (TMOS) were slowly added and the "sol" was stirred again for 4 h. Finally, the sol was poured in closed containers and kept in an oven at 50 °C. Gelation occurred in 6 days. Then gel was dried as xerogel for about 2 weeks at 50 °C.

2.2 Preparation of pre-functionalized 2SiO₂–B₂O₃ xerogel (sample SiBNH2)

10.39 g of TMB were dissolved in 15 ml of methanol and 3.6 ml of $\rm H_2O$ and stirred for 1 h in order to complete the hydrolysis stage. Then 11.41 g of TMOS were slowly added and the sol was stirred for 1 h. Separately, 5.53 g of aminopropyltriethoxysilane (APTES) which is 25 % mol of the total Si, were added to 10 ml of ethanol and 1.35 ml of $\rm H_2O$ and stirred for 1 h. Finally, the sol of APTES was slowly added to the first sol which turned opaque and gelation occurred in 10 min. The gels were dried for about 3 weeks in an oven at 50 °C.

2.3 Top-down method for nanoparticles (NPs) production

Xerogel samples were ground manually in an agate mortar and afterwards milled by a high performance planetary milling machine (FRITSCH Pulverisette 7) with speeds ranging between 300 and 850 rpm, by repeating 24 times the cycle run = 30 min; pause = 20 min.

2.4 Functionalization of NPs with folic acid (sample SiBNH2_F)

2.65~g of folic acid were dissolved in 15~ml of dry dimethylsulfoxide (DMSO) in a 100~ml round bottom flask under N_2 atmosphere, then 2.3~g of 1-ethyl-3-(3-dimethylaminopropyl)carbodiimide hydrochloride (EDC), 0.69~g of N-hydroxy succinimide (NHS) and 0.5~ml of pyridine were added. The reaction mixture was stirred at room temperature for 1~h. Then 3~g of glass nanoparticles were added to the flask and the reaction mixture was kept overnight under magnetic stirring. The mixture was then filtered on suction and the resulting yellowish residue was washed twice times with DMSO under sonication, then twice in water and acetonitrile under sonication and then centrifuged. The final NPs were obtained upon washing with ethyl alcohol and acetone followed by centrifugation



and dryness. This cumbersome washing procedure was necessary to remove the folic acid adsorbed on the nanoparticles surface, accounting as much as 25 wt % without washing (TGA analysis, data not shown).

2.5 ICP-OES analysis

About 60 mg (exactly weighed) of each sample, were digested overnight at room temperature with 0.2 ml 40 % HF and 0.2 ml 65 % HNO₃ in a closed PET vessel and then diluted with milliQ water to 50 ml. The boron concentration in the digested samples, diluted 1:10, was measured by inductively coupled plasma spectroscopy (ICP-OES). An ICP-OES Perkin Elmer Optima 3300 DV was used for all the measurements, following the operating conditions suggested by the manufacturers (in radial view). A linear relationship between the signal intensity and boron concentration (0.030-20 mg l⁻¹) was obtained by using standard solutions daily prepared from a 1.001 mg ml⁻¹ stock solution. LOD = $10 \mu gL^{-1}$, LOQ = $30 \mu gL^{-1}$. All data were corrected in order to take into account the humidity of the sample. The water content was determined by TGA analysis.

2.6 Thermal analysis

Thermogravimetric scans were performed by a TGA 2950 (TA Instruments) under O₂ purge, at a heating rate of 5 °C/min, from room temperature up to 900 °C. Differential scanning calorimetry measurements were carried out by means of a 2910 DSC (TA Instruments) under O₂ purge at 5 °C/min from room temperature up to 300 °C. The upper limited temperature was chosen to prevent cell contamination during sample decomposition.

2.7 FT-IR spectroscopy

Reflectivity spectra were obtained between 600 and 4000 cm⁻¹ by using a FT-IR 410 JASCO spectrometer. The samples were finely mixed with KBr (about 5 wt % of sample), and the spectra were obtained by subtraction with a blank one (pure KBr). The signals were averaged over 512 scans, with a resolution of 2 cm⁻¹ and a scan velocity of 2 mm/s. Spectra were reported as transmittance mode.

2.8 Solid state NMR

 13 C $\{^{1}$ H $\}$ CPMAS NMR spectra were acquired by means of a Bruker Avance Spectrometer II 400 (9.4 T), with a MAS frequency of 13 kHz, a 1 H 90° pulse at of 4.2 μ s, contact time of 1.5 ms, delay time of 4 s and 4000 acquisitions. Hartman-Hahn condition was optimized on a standard of adamantane.



Microphotographs were collected with a Zeiss EVO-MA10 (Carl Zeiss, Oberkochen, Germany) on gold sputtered samples.

2.10 Preparation of NP suspensions

NPs were suspended in phosphate buffer saline (PBS, 5 mM sodium phosphate at pH 7.4, 154.5 mM NaCl, 4.5 mM KCl) at the concentration of 3 mg/ml. An ultrasound treatment of 5 min were performed three times to deagglomerate homogeneously the NPs, using a probe sonication device (Soniprep 150, Sanyo).

2.11 Analysis of platelet aggregation

Platelet aggregation analysis was performed as previously described [20]. Briefly, 0.3-ml samples of washed human platelets at the final concentration of 3×10^8 cells/ml were stimulated with the reported doses of NPs in a Born lumiaggregometer at 37 °C in the presence of 1 mM CaCl₂. Platelet aggregation, measured as the variation of light transmission, was monitored for 5 min.

2.12 Analysis of neutrophil activation

Neutrophils were obtained from human venous blood by Dextran-70 sedimentation followed by Ficoll-Hypaque gradient centrifugation, essentially as described in [21] and washed in PBS supplemented with 2 mM EDTA, 0.5 % (w/v) bovine serum albumin and 0.1 % (w/v) glucose. The residual erythrocytes in the neutrophil-rich fraction were eliminated by differential hypotonic lysis. The samples for the assay (150 µl, final volume) were prepared as shown below (final concentrations): neutrophils $(2 \times 10^4 \text{ cells})$ μl), luminol (10 μM), sodium phosphate pH 7.4 (5 mM), NaCl (154.5 mM), KCl (4.5 mM), MgCl₂ (1 mM), CaCl₂ (0.6 mM). After the addiction of NPs (1 mg/ml) or phorbol myristate acetate (PMA, 0.8 µM), neutrophil activation was monitored by luminol-enhanced chemiluminescence method in a 96-wells microtiter plate reader (Genios Plus, Tecan) for 60 min, at 37 °C and under stirrer. The samples were made in quadruplicate (Fig. 1).

3 Results and discussion

Sol–gel synthesis, as expected, leads to a sample with a low boron content: the amount of boron, as analyzed by ICP-OES, was 1.2 wt %. Considering that the theoretical amount should be 11.4 wt % (B as B_2O_3), the boron loss is about 89 %. Sol–gel synthesis of a prefunctionalized system



Fig. 1 Reaction of functionalization of borosilicate nanoparticles with folic acid

2SiO₂-B₂O₃, with the presence of -CH₂CH₂CH₂NH₂ groups gave an experimental boron content of about 4.4 wt %. In this case, the theoretical amount of B is about 8 wt %, then boron loss is strongly reduced (about 45 % compared to 89 %). After functionalization with folic acid. the final amount of B is 2.7 wt %, which means that a significant further boron loss does not occur in the functionalization procedure (see TGA results). Figure 2 shows the TGA data of the following samples: (1) SiB; (2) SiBNH2; (3) SiBNH2 F. Non-functionalized SiB sample exhibits a total weight loss of about 13 % at 800 °C, the first single-step weight decrease below 200 °C is due to the moisture removal and eventual trimethoxyborate evaporation, while the second continuous weight decrease could be due to condensation of -OH groups, a typical feature of xerogel samples. The pre-functionalized SiBNH2 sample shows a weight loss of 26.5 % at 800 °C. Similar considerations as for SiB can be made at low temperatures, whereas the more evident step decrease between 300 and 600 °C could be ascribed to decomposition of the -CH₂CH₂CH₂NH₂ groups. By considering the difference in moisture content between SiBNH2 and 2SiB, one can estimate an experimental loss of the organic part of about 10–11 wt %, compared to a theoretical value ranging around 13 wt %. The SiBNH2_F sample exhibits a total weight loss of about 42 %, which this value is compatible with the 50 wt % expected if admitting that all the –NH₂ groups do react with folic acid. Figure 3 reports the DSC data of the same three samples. The non-functionalized sample 2SiB exhibits a broad endothermic peak up to ≈ 200 °C related to moisture removal, and no apparent events can be detected at least up to 300 °C. The pre-functionalized SiBNH2 sample shows the endothermic effect due to moisture release around 100 °C, followed by an exothermic feature at ≈ 250 °C likely due to incipient decomposition of the CH₂CH₂CH₂NH₂ groups. The functionalized SiBNH2_F sample displays a tiny endotherm below 150 °C corresponding to the little amount of moisture contained in such a specimen, which is more hydrophobic thanks to the presence of folic acid. Even in this case, the exothermic profile above 200 °C can be related to incipient decomposition of the organic part.

The functionalization reaction was firstly monitored by IR spectroscopy. Figure 4 shows the IR spectra of the prefunctionalized sample SiBNH2, the functionalized one and the folic acid. For SiBNH2 sample the broad band between 1300 and 1500 cm⁻¹ is due to the stretching of B–O bonds where B is in planar trigonal coordination, whereas the second broad band between 1000 and 1200 cm⁻¹ is due to both the Si–O–Si and B–O–B groups. Some very weak bands between 2300 and 2500 cm⁻¹ can be attributed to the borate group. In fact, our previous study [15] showed that when [B] is less than 3 wt % it is very difficult to detect the six typical borate bands in this region. The band at 3200 cm⁻¹, corresponding to the -OH stretching of B–OH, is slightly evident inside the broad band between 3200 and 3700 cm⁻¹ due to the OH stretching of both



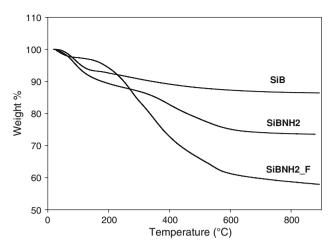


Fig. 2 TGA traces of samples SiB, SiBNH2 and SiBNH2_F

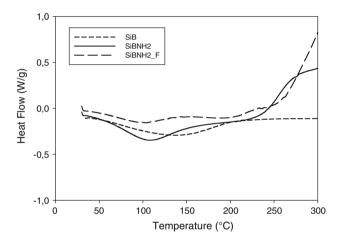


Fig. 3 DSC traces of samples SiB, SiBNH2 and SiBNH2_F

silanol groups and water. The band at around 1635 cm⁻¹ confirms the presence of free water molecules. Unfortunately, some typical signals of the group –NH₂ could not be detected because they were completely masked by those of free-water and –OH groups. The presence of signals due to the –CH₂CH₂CH₂NH₂ groups is mixed with the above cited broad band between 1000 and 1200 cm⁻¹.

The IR spectrum of the folic acid is very complex, the signals are not completely assigned, and there is not full agreement in the literature about the interpretation of some bands. For example He et al. [22] ascribed the bands between 3400 and 3600 cm⁻¹ both to –OH stretching of the glutamic acid portion and to –NH stretching of the pterinic portion. Then, bands between 1510 e 1485 cm⁻¹ are due to the C–C vibrations of phenolic and pterinic ring. The same authors ascribed the broad and complex band at 1696 cm⁻¹ to the stretching of different –C=O groups, and the band at 1607 cm⁻¹ to the bending of –NH groups. In contrast, Yang et al. [23] assigned both the band at 1607 cm⁻¹ and the band at 1449 cm⁻¹ to the stretching of

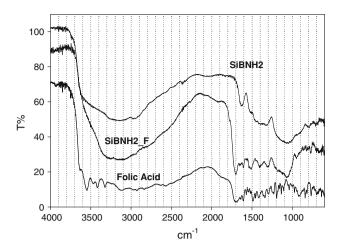


Fig. 4 FT-IR spectra of folic acid and samples SiBNH2 and SiBNH2 F

aromatic C=C bonds. Vora et al. [24] assigned the bands between 2860 and 2960 cm⁻¹ to the symmetric and antisymmetric stretching of C-H bonds. All the cited authors agreed in assigning the multiple band at 1696 cm⁻¹ to the stretching of different -C = O groups. The IR spectrum of sample SiBNH2_F, in particular the region between 1200 and 1700 cm⁻¹ indicates the presence of folic acid but it is very difficult to detect the formation of the new -NHCObond. In fact, a secondary amide group is still present in the folic acid molecule and it is impossible to distinguish it from the new one (also secondary). A similar consideration can be done with respect to the broad signal of the -COOH group which becomes a -NHCO group, because it falls in the same frequency region of the other -COOH group. which does not react because sterically hindered and engaged by means of a H-bond (see below).

From these spectra it is possible to state that folic acid is present on the surface of borosilicate NPs, but it is not possible to prove the occurred reaction. Additional information can be obtained by solid-state NMR. Figure 5 reports the CPMAS NMR spectrum of folic acid. According to the SDBS-¹³C NMR data base the carbon signals can be easily assigned (see inset of Fig. 5). In particular signals no 1 and no 2 refer to the carboxylic groups. Figure 6 reports the NMR spectrum of the sample SiBNH2. As expected only three signals are evidenced, which are due to the three carbons of the -CH2CH2CH2NH2 group as showed in the inset scheme. Figure 7 shows the NMR spectrum of the NPs functionalized with folic acid. As expected, the signals related to the organic shell of the inorganic borosilicate particle are broader compared to those presented in Fig. 5. The peaks belonging to CH₂CH₂CH₂NH₂ are clearly visible (A, B, C), whereas the peak marked with X is probably due to residual DMSO adsorbed on the particles due to its high boiling point (189 °C). The signals related to folic acid are



Fig. 5 Solid state ¹³C { ¹H} CPMAS NMR of folic acid

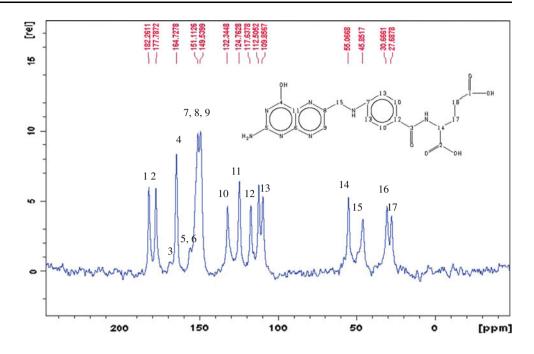
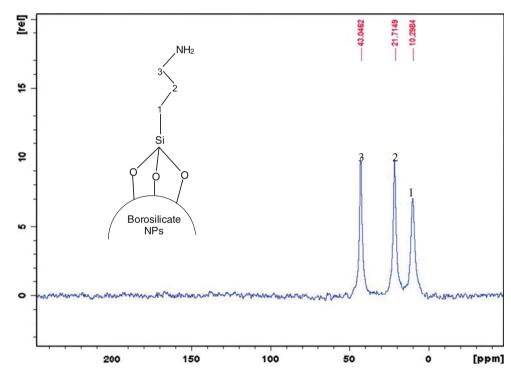


Fig. 6 Solid state ¹³C { ¹H} CPMAS NMR of sample SiBNH2



still observable although less definite. The most important difference, indeed, is that signal at about 182 ppm (no 1) related to the reacted carboxylic group disappears, while that signal no 2 related to the second carboxylic group is still present. This occurrence proved that reaction showed in Fig. 1 (the formation of an amide bond) really took place.

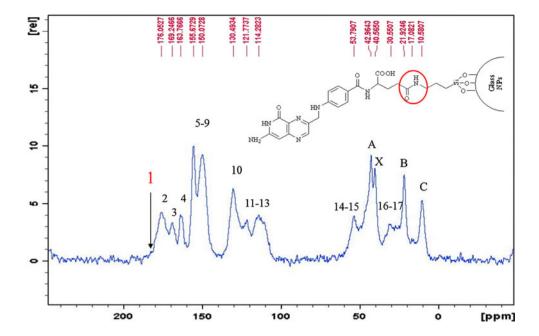
For what concerns the particle size, Fig. 8a, b shows the SEM microphotographs of milled pre-functionalized NPs (SiBNH2 sample) and functionalized NPs (SiBNH2_F

sample), respectively. Both the samples consist of aggregates of rounded particles. The average diameter of SiB-NH2 particles ranges between 100 and 200 nm, while the average diameter of SiBNH2_F particles appears slightly greater, probably because of the functionalization with folic acid on the surface.

As mentioned above, BNCT requires the infusion in the bloodstream of the boron-carrying drug, hence, in order to be suitable for this therapy, the borosilicate NPs must offer



Fig. 7 Solid state ¹³C { ¹H } CPMAS NMR of sample SiBNH2_F



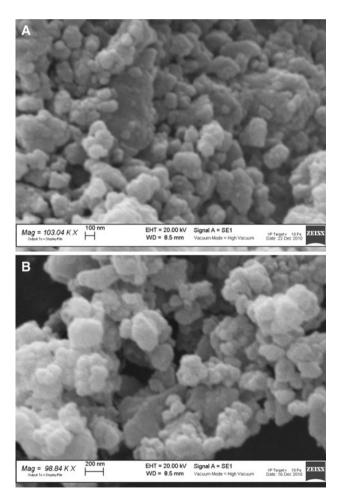


Fig. 8 SEM micrographs of samples SiBNH2 (a) and SiBNH2_F (b)

a high level of haemocompatibility. Unfortunately, many types of nanomaterials are effective to stimulate different blood cell types. We focussed our attention on the effects of NPs on platelets and neutrophils. Platelets are key actors in physiological haemostasis, but uncontrolled or unnecessary platelet activation stimulates platelet aggregation and subsequent thrombus formation, which leads to the infarction of the tissues downstream of the occluded vessel [25]. Therefore, ideally, NPs used in BNCT should be completely ineffective in stimulating platelets. In Fig. 9a it is reported that SiBNH2 at the dose of 100 µg/ml is able to induce a strong platelet aggregation, that is even more evident when the NPs are used at the dose of 500 µg/ml. Interestingly, the functionalization with folic acid completely abolished the pro-aggregating activity of NPs, as SiBNH2_F is unable to induce platelet aggregation at both tested doses.

Neutrophils are involved in the innate immunity system and in the inflammatory processes, engulfing the microorganisms and killing it by the release of proteolytic enzymes and several strong oxidative species. Uncontrolled neutrophil activation can induce several inflammatory-dependent diseases [26]. For this reason, the NPs proposed as boron-carrier for BNCT should be totally inert to neutrophils. In Fig. 9b we showed the luminol-enhanced chemiluminescence produced by reaction with the oxidative species released from neutrophils activated by incubation with NPs. The treatment with SiBNH2, at the dose of 1 mg/ml, induces a strong neutrophil activation, comparable to that observed during PMA stimulation, a typical



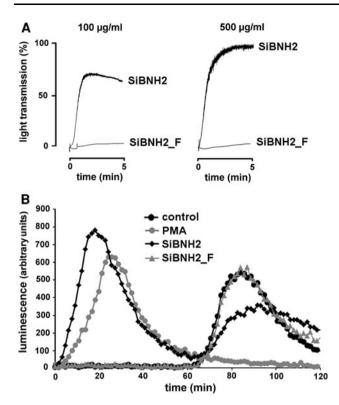


Fig. 9 a Aggregation of human platelets stimulated for 5 min with SiBNH2 and SiBNH2_F (100 and 500 μg/ml) in a Born aggregometer at 37 °C under constant stirring. Aggregation was measured continuously as increase of light transmission. **b** Luminol-induced chemiluminescence of human neutrophil non-stimulated (control), or treated with: SiBNH2, SiBNH2_F and PMA. Following one hour of incubation, the samples "control", "SiBNH2" and "SiBNH2_F" were added with PMA, and the chemiluminescence was monitored for another hour

neutrophil activator. Conversely, the treatment with the same dose SiBNH2_F does not induce neutrophil activation. To verify if the apparent lack of pro-inflammatory property of SiBNH2_F was conversely due to a cell death during incubation, PMA was added to the samples (excepted the one already treated with PMA) and chemiluminescence was monitored again, showing that neutrophils pre-treated with SiBNH2_F have the same intensity of activation of untreated neutrophils (control). Both cytotoxic and pro-inflammatory properties of functionalized NPs were thus excluded. Borosilicate NPs are not cytotoxic for neutrophils at the concentration used in these experiments, but SiBNH2 have a high pro-inflammatory property that is completely abolished by functionalization with folic acid.

4 Conclusions

Borosilicate NPs were obtained by means of a top-down approach from a suitable xerogels system. NPs were

successfully functionalized with folic acid. The procedure of pre-functionalization of NPs with amino groups solved two problems at the same time: the boron leaching and subsequent functionalization with folic acid. The functionalization of NPs does not significantly increase the boron loss, and the final amount of B in the particles is 2.7 wt %. By considering that standard BPA has a boron content of about 5.1 wt %, this amount is acceptable for biological tests. Moreover, it can be upgraded if different xerogel system as SiO₂–2B₂O₃ are prepared [15].

The tests performed on blood cells showed that the functionalization of NPs with folic acid, introduced to increase NP incorporation in the tumor cells, also provided an important additional advantage in terms of haemocompatibility. Indeed, although SiBNH2 was able to induce platelet aggregation and neutrophil activation, SiBNH2_F resulted essentially ineffective in activating both cell types.

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References

- Soloway AH, Tjarks W, Barnum BA, Rong FG, Barth RF, Codogni IM, Wilson JG (1998) Chem Rev 98:1515–1562
- 2. Tiwari SB, Amiji MM (2006) Curr Drug Deliv 3:219-232
- 3. Goldberg M, Langer R, Jia X (2007) J Biomater Sci Polym 18:241–268
- 4. Low PS, Kularatne SA (2009) Curr Opin Chem Biol 13:256-262
- Yang X, Grailer JJ, Pilla S, Steeber DA, Gong S (2010) Bioconjugate Chem 21:496–504
- Ciofani G, Raffa V, Menciassi A, Cuschieri A (2009) Nanoscale Res Lett 4:113–121
- 7. Yao A, Wang D, Fu Q, Huang W, Rahaman MN (2007) Chin Sci Bull 52(2):272–276
- 8. Nogami M, Moriya Y (1982) J Non-Cryst Solids 48:359-366
- Irwin AD, Holmgreen JS, Zerda TW, Jonas J (1987) J Non-Cryst Solids 89:191–205
- Irwin AD, Holmgreen JS, Jonas J (1988) J Non-Cryst Solids 101:249–254
- 11. Li B, Yue Z, Zhou J, Gui Z, Li L (2002) Mater Lett 54:25-29
- Soraru GD, Dallabona N, Gervais C, Babonneau F (1999) Chem Mater 11:910–919
- Soraru GD, Babonneau F, Gervais C, Dallabona N (2000)
 J Sol-Gel Sci Technol 18:11-19
- Parashar VK, Orhan JB, Sayah A, Cantoni M, Gijs MAM (2008) Nat Nanotechnol 3:589–594
- Grandi S, Tomasi C, Cassinelli V, Cucca L, Profumo A, Mustarelli P, Balduini C (2012) SiO₂-B₂O₃ xerogels: the problem of boron leaching. J Non Cryst Solids 358(14):1631–1637
- 16. Nel A, Xia T, Mädler L, Li N (2006) Science 311:622-627
- 17. Oberdörster G (2010) J Intern Med 267:89-105
- Bartneck M, Keul HA, Singh S, Czaja K, Bornemann J, Bockstaller M, Moeller M, Zwadlo-Klarwasser G, Groll J (2010) ACS Nano 4:3073–3086
- Radomski A, Jurasz P, Alonso-Escolano D, Drews M, Morandi M, Malinski T, Radomski MW (2005) Br J Pharmacol 146:882–893



- Guidetti GF, Consonni A, Cipolla L, Mustarelli P, Balduini C, Torti M (2012) Nanomedicine. doi:10.1016/j.nano.2012.04.001
- Melloni E, Pontremoli S, Michetti M, Sacco O, Sparatore B, Salamino F, Horecker BL (1985) Proc Natl Acad Sci USA 82:6435–6439
- 22. He YY, Wang XC, Jin PK, Zhao B, Fan X (2009) Spectrochimica Acta Part A 72:876–879
- Yang SJ, Lin FH, Tsai FC, Wei MF, Tsai HM, Wong JM, Shieh MJ (2010) Bioconjugate Chem 21:679–989
- 24. Vora A, Riga A, Dollimore D, Alexander KS (2002) Thermochimica Acta 392–393:209–220
- 25. Gawaz M, Langer H, May AE (2005) J Clin Invest 115: 3378–3384
- 26. Malech HL, Gallin JI (1987) N Engl J Med 317:687-694

