

Human Movement Science

Dynamic Networks of Physiologic Interactions of Brain Waves and Rhythms in Muscle Activity

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Abstract:	<p>The brain plays a central role in facilitating vital body functions and in regulating physiological and organ systems, including the skeleto-muscular and locomotor system. While neural control is essential to synchronize and coordinate activation of various muscle groups and muscle fibers within muscle groups in relation to body movements and distinct physiologic states, the dynamic networks of brain-muscle interactions have not been explored and the complex regulatory mechanism of brain-muscle control remains unknown. Here we present a first study of network interactions between brain waves at different cortical locations and peripheral muscle activity across key physiologic states – wake, sleep and distinct sleep stages. Utilizing a novel approach based on the Network Physiology framework and the concept of time delay stability, we find that for each physiologic state the network of cortico-muscular interactions is characterized by a specific hierarchical organization of network topology and network links strength, where particular brain waves are main mediators of interaction and control of muscular activity. Further, we uncover that with transition from one physiological state to another, the brain-muscle interaction network undergoes marked reorganization in the profile of network links strength, indicating a direct association between network structure and physiological state and function. The pronounced stratification in brain-muscle network characteristics across sleep stages is consistent for chin and leg muscle groups and persists across subjects, indicating a remarkable universality and a previously unrecognized basic physiologic mechanism that regulates muscle activity even during rest and in the absence targeted direct movement. Our findings demonstrate previously unrecognized coordination between brain waves and activation of different muscle fiber types within muscle groups, laws of brain-muscle cross-communication and principles of network integration and control. These investigations demonstrate the potential of network-based biomarkers for classification of distinct physiological states and conditions, for the diagnosis and prognosis of neurodegenerative, movement and sleep disorders, and for developing efficient treatment strategies.</p>
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Experience in:

complex systems
data analysis
network neuroscience
network physiology
signal processing

Highlights

- Network Physiology approach to brain-muscle interactions reveals complex networks.
- Time delay stability measure identifies coupling of brain waves with muscle rhythms.
- Hierarchical organization in brain-muscle networks with distinct profiles of links strength.
- Distinct profiles for network links strength during wake, sleep and sleep stages.
- Brain-muscle network universality for different muscle groups and subjects.

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**Dynamic Networks of Physiologic Interactions
of Brain Waves and Rhythms in Muscle Activity**

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Abstract

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Dynamic Networks of Physiologic Interactions of Brain Waves and Rhythms in Muscle Activity

1. Introduction

The human body comprises diverse organ systems, which continuously interact to synchronize and coordinate their dynamics and to generate various physiological functions. Mapping the network of interactions among physiological systems is thus of primary importance to fully understand basic physiological states and functions, to rigorously define and discriminate between healthy and pathological conditions. A new field, Network Physiology (Ivanov, 2021; Ivanov, Liu & Bartsch, 2016), has been established to address the fundamental question of how physiological states and functions emerge at the organism level through integrated networks of interactions among diverse systems and subsystems across spatiotemporal scales (Bashan et al., 2012; Bartsch et al., 2015; Ivanov & Bartsch, 2014). In this context, the brain-muscle communication network, which is essential for locomotor control of posture and movements during distinct physiologic states, remains not understood. Traditional approaches to cortico-muscular coordination focus on associations between movement tasks or exercises and the activation of particular brain waves at specific cortical areas (Ciria et al., 2019; Rendeiro & Rhodes, 2018; Yokoyama et al., 2016). However, neural control of the muscular system is continuously present even at rest. Recent studies have shown that network interactions among brain waves are characterized by distinct coupling profiles and network plasticity that are essential to generate physiological states and functions (Lin et al., 2020; Bartsch & Ivanov, 2022; Liu et al., 2015a,b). We hypothesize that network interactions between

95 brain waves and rhythms embedded in muscle activity may also reflect changes in
96 physiologic regulation as a function of physiological states. We investigate the coupling
97 between physiologically relevant brain waves at distinct cortical locations with peripheral
98 EMG activity in different frequency bands across four major, well defined physiological
99 states — Wake, REM, Light Sleep (LS), Deep Sleep (DS). We aim to map the default
100 brain-muscle interaction network corresponding to low level of physical activity in the
101 absence of directed and targeting movements during sleep and quiet restful wake.
102 Importantly, we find that cortico-muscular interaction profiles of network links strength
103 and related network topology uniquely identify each physiological state and hierarchically
104 reorganize with transition from one state to another – wake to sleep and across sleep
105 stages.

106 2. Methods

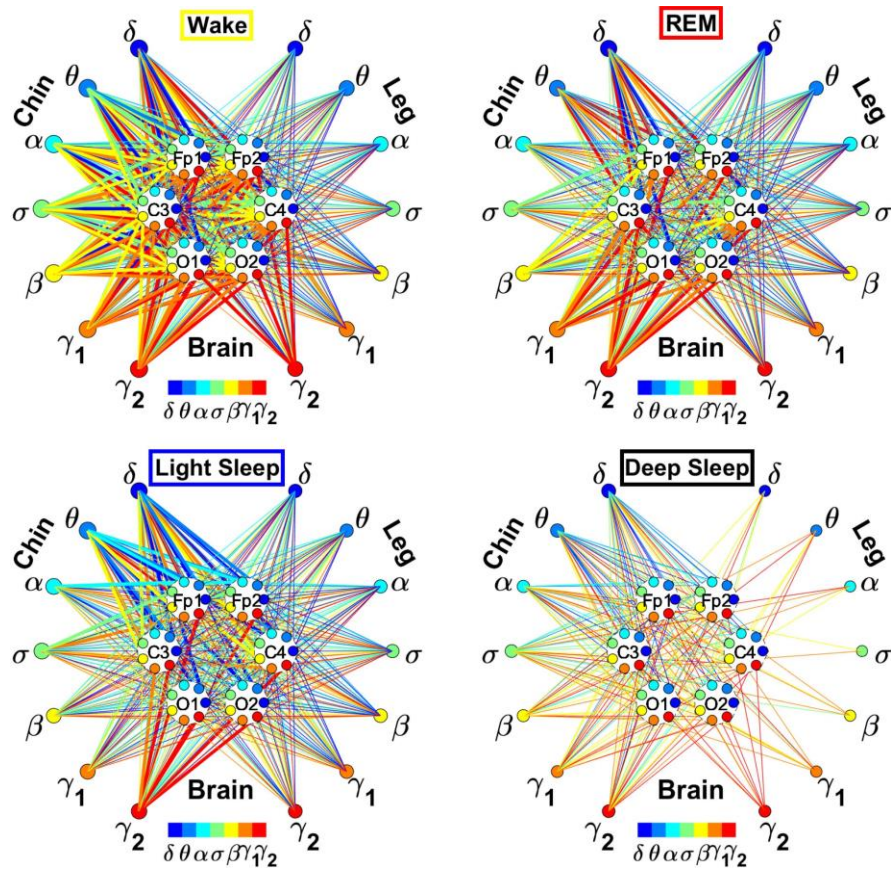
107 2.1. Data

108 We analyze cortical EEG and surface leg and chin muscle EMG signals from 36
109 healthy young subjects (ages 20-40, $M = 29$ years old), synchronously and continuously
110 recorded during nocturnal sleep (ave. record duration 7.8h) from EU SIESTA databases
111 (Klosh et al., 2001). Data were divided in 30 s epochs and scored as Wake, REM, LS and
112 DS (Klosh et al., 2001). Analyzed data include EEG from six scalp locations (Fp1, Fp2,
113 C3, C4, O1, O2) and the EMG of left leg muscle (anterior tibialis) and chin muscle
114 (mentalis). Data were visually inspected to remove noisy segments, usually located at the
115 beginning and the end of the recordings. Power-line interferences were removed using a
116 50 Hz notch filter, and signals were bandpass filtered in the range [0.5 98.5] Hz. The
117 spectral power of seven frequency bands of the EEG and EMG signals was parallelly
118 extracted in moving windows of 2s with a 1s overlap: δ [0.5–3.5] Hz, θ [4–7.5] Hz, α [8–

119 11.5] Hz, σ [12–15.5] Hz, β [16–19.5] Hz, γ_1 [20–33.5] Hz and γ_2 [34–98.5] Hz. Thus, all
120 time series have the same time resolution of 1s before the analysis.

121 **2.2. Time Delay Stability**

122 We use the Time Delay Stability (TDS) method (Bashan et al., 2012) to quantify
123 periods of synchronous activity in two systems, where bursts in one system are followed
124 with constant time delay by bursts in the other system, as a measure of degree of
125 coupling. TDS quantifies the stability of the time delay with which bursts in the output
126 dynamics of a given system are consistently followed by corresponding bursts in the signal
127 output of another system. Longer periods of TDS between the output signals of two
128 systems reflect more stable interaction and stronger coupling. Strong coupling (high TDS)
129 between two systems corresponds to a strong link in the interaction network between brain
130 waves and muscle activity rhythms. Network link strength is defined as %TDS, i.e., the
131 fraction of segments with TDS (constant time delay) in the entire recording. To test the
132 statistical significance and physiological relevance of the network interactions identified by
133 the TDS method, we perform a surrogate test: for each link in a given sleep stage, 200
134 surrogates are generated considering signals from two randomly chosen subjects, and a
135 surrogate average link strength (%TDS) is obtained. The procedure is repeated for each
136 network link to obtain a distribution of surrogate link strengths for each sleep stage.
137 For each distribution the mean μ_{surr} and standard deviation σ_{surr} are estimated. Thus,
138 the significance threshold at 95% confidence level for the network link strength is
139 defined as $\mu_{surr} + 2\sigma_{surr}$ corresponding to %TDS = 2.3%, and is represented by
140 horizontal green lines in all figure panels showing bar plots of average link strength.
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142

143 **Figure 1**

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145 **2.3. Averaging procedure for estimating links strength in physiological networks**

146 For each physiologic state, we calculate a group-average %TDS representing the
 147 coupling of each leg/chin EMG frequency band with the brain waves (cortical rhythms)
 148 embedded in each EEG channel across all subjects. To avoid coupling artifacts related to
 149 noisy data in the calculation of the group-average TDS for each network link, we remove
 150 outlier subjects for which the strength of the link is outside ± 2 standard deviation of the
 151 group-average TDS, and we recalculate the new updated group-average link strength.

152 In the cortico-muscular network (Fig. 1), group-average TDS link strength is
 153 represented by the link thickness. To obtain information on the average link strength

154 representing the interaction of a brain wave from a given brain area with all EMG rhythms
155 (integrated EMG activity), we calculate the average coupling strength (%TDS) of a given
156 brain wave from a given EEG channel with all EMG bands of the leg (or chin) muscle (Fig.
157 2). Similarly, to obtain information on the relative contribution in the brain-muscle
158 communication network of each muscle activity rhythm (EMG frequency band) with the
159 integrated EEG activity, we consider the average coupling strength of a given EMG
160 frequency band with all brain waves at a given EEG channel location (Fig. 3). We refer
161 to these two types of coarse-grained networks as 'brain waves to integrated muscle activity'
162 and 'muscle rhythms to integrated brain activity' interaction networks.

163 3. Results

164 3.1. Brain-muscle network and its dynamical reorganization across physiologic states

165 We identify and characterize the brain-muscle interactions network across four
166 major physiologic states: Wake, REM, LS and DS. We consider brain activity from six
167 major cortical areas — Fp1, Fp2, C3, C4, O1, and O2 —, leg muscle tone, and chin
168 muscle tone, simultaneously recorded overnight-sleep using EEG and EMG. We then
169 quantify couplings and network interactions by means of the TDS method [1]. The
170 cortico-muscular network in Fig. 1 reorganizes across physiologic states. Specifically, the
171 network is denser and exhibits stronger links during Wake, and sparser during LS and DS.
172 Brain-chin network links are generally stronger than brain-leg links, in particular during
173 Wake and REM. Particular cortical rhythms and EMG frequency bands emerge as main
174 mediators of the brain-muscle interaction. During Wake and REM the strongest links
175 correspond to interactions mediated by the high frequency cortical rhythms, in particular
176 γ_2 (red links). We observe that the network markedly reorganizes with transition to LS,
177 and strong links related to slower cortical rhythms appear in the network (dark and light

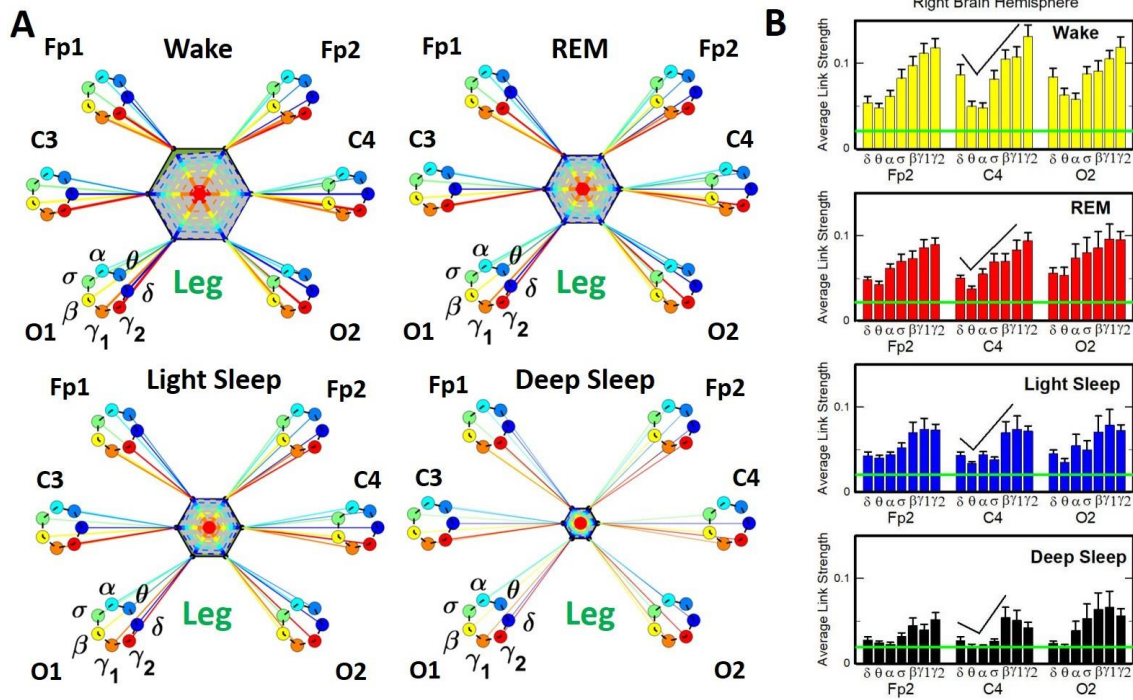
178 blue links), in particular between the chin and the frontal region of the brain. Finally, the
179 link number and strength abruptly decline during DS (Fig. 1).

180 **3.2. Coarse-grained interaction networks of cortical rhythms with integrated leg** 181 **muscle tone**

182 To identify the role of different brain rhythms in muscle control across cortical lo-
183 cations, we coarse-grain the TDS links strength across EMG rhythms (Sect. II), and
184 represent in coarse-grained networks and corresponding bar charts (Fig. 2). The brain-leg
185 interaction network significantly changes with transition across sleep, with strong
186 interactions during Wake, intermediate during REM and LS, and weak during DS (One-
187 Way ANOVA rank test for each brain location shows a statistically significant
188 difference between sleep stages; $p < .001$). No significant differences in network links
189 strength are found between the left and right hemisphere for each sleep stage (MW
190 test, $p > .67$), nor among different brain areas within a brain hemisphere for a given sleep
191 stage (One-Way ANOVA rank test; $p > .44$). The frequency profile of network links
192 remains stable for all brain areas in a given sleep stage, and reorganizes with transitions
193 across sleep stages. During Wake, brain-to-leg interaction is characterized by strongest
194 links for the high-frequency bands γ_1 and γ_2 and a gradual decrease in links strength for
195 the lower-frequency bands, followed by a slight kink up in link strength for the δ band
196 (One-Way ANOVA rank test and multiple pairwise comparison performed for Fp1 show
197 $p < .005$). Differences between links involving different cortical rhythms gradually
198 decrease in REM, LS and DS, although remaining significant. Similar patterns in the
199 network structure and frequency profile reorganization are observed for brain-chin
200 interactions.

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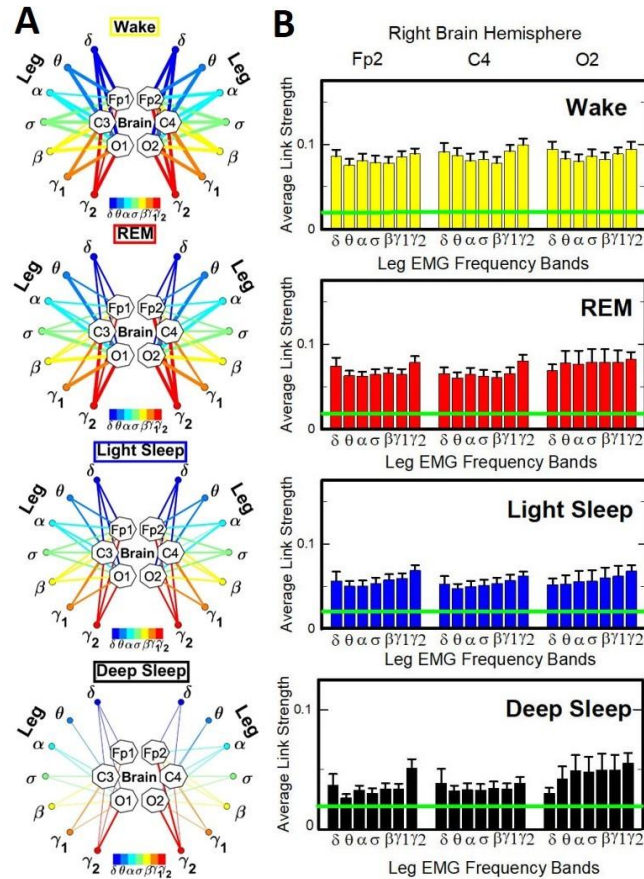
Figure 2

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206 3.3. Coarse-grained interaction networks of integrated brain activity at cortical 207 locations and leg EMG frequency bands

208 We next consider the average coupling strength of a given EMG frequency
209 band with all brain waves derived from an EEG channel (Fig. 3). The leg-brain network
210 reorganizes across states, with uniform distribution of links over cortical areas, and a
211 symmetry between left and right hemispheres. In contrast to brain-to-leg network, we do
212 not observe dominant links in the interactions of leg EMG bands with integrated cortical
213 areas for all sleep stages (One-way ANOVA $p > .21$). Links are stronger during Wake,
214 with decreasing strength for REM, LS and DS. Chin-to-brain networks exhibit similar
215 stratification and reorganization across sleep stages.

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218 **Figure 3**

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220 4. Discussion

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We systematically study brain-muscles interaction networks and their associations with physiologic states. We find that neuromuscular control is mediated through complex network interactions between brain waves and rhythms in muscle activity, with hierarchical organization of network links strength as a hallmark of physiologic state. The reported results are robust and consistent across subjects indicating universal laws in brain-muscle network communication. Furthermore, we uncover preferred pathways in network communication between brain waves and rhythms in the skeletal muscles activity that

228 uniquely identify sleep stages through a previously unrecognized hierarchical network
229 organization. The reported findings open new perspectives on the regulatory mechanisms
230 of brain dynamics and neuromuscular activity in the absence of directed and targeted
231 movement during quiet wake and sleep. They show that in addition to neural synchrony
232 within the motor system (Wijk, Beek, & Daffertshofer), synergy among muscle groups
233 (Bach, Daffertshofer, & Dominici; Kerkman et al., 2020) and activation of brain waves
234 across cortical areas during active movement (Ciria et al., 2019), there is a previously
235 unrecognized physiologic mechanism regulating network interactions between brain
236 waves and rhythms in muscle activity. These investigations raise new questions of how
237 cortical waves and spectral rhythms in muscle activity representing different types of
238 muscle fibers (Garcia-Retortillo et al., 2020; Garcia-Retortillo, Rizzo & Ivanov, 2021)
239 synchronize and integrate as a network during exercise and breakdown with fatigue
240 (Balagué et al., 2020). Further, our study shows that different brain waves play role as the
241 main mediators of brain-muscle network interactions compared to the brain-heart
242 regulatory network (Lin et al., 2016), which demonstrates that markedly different dynamic
243 networks with distinct structure and dynamics mediate autonomic regulation and brain
244 control of different organ systems (Ivanov et al., 2017). The reported empirical
245 observations of hierarchical reorganization in brain-muscle networks with transitions
246 across states, where distinct profiles of network links strength represent each physiologic
247 state, indicate the potential utility of the Network Physiology framework and derived
248 network-based novel biomarkers with implications for neurodegenerative, locomotor and
249 sleep disorders (Moorman, Lake & Ivanov, 2016).

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253

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design, data collection and analysis, decision to publish, or preparation of the manuscript.

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351 **Figure captions**

352 *Figure 1.* Dynamic networks of cortico-muscular interactions across physiological states.
353 Network maps represent physiological interactions during wake, REM, LS and DS. Brain
354 areas are represented by two Frontal, two Central and two Occipital EEG channels, where
355 nodes with different color in each brain area represent distinct brain waves. Peripheral
356 nodes indicate EMG frequency bands of leg and chin muscle tone shown in the same color
357 as the brain waves. Network links show the coupling strength of each cortical rhythm
358 across cortical areas with each EMG frequency band as quantified by the TDS measure.
359 Links strength is marked by line width: thin lines for $3\% < \%TDS < 12\%$; thick lines
360 for $\%TDS > 12\%$. TDS = Time Delay Stability.

361
362 *Figure 2.* Dynamic network interactions between cortical rhythms and integrated leg-
363 muscle activity across physiological states. (A) Radar-chart representation of group-
364 averaged TDS coupling strength of the interactions between each brain rhythm at a given
365 cortical location and the leg muscle tone, after averaging over all leg EMG frequency
366 bands. Brain areas are represented by six EEG channels, where network nodes with
367 different colors mark different cortical waves. A centered hexagon represents the
368 integrated leg muscle tone. Links strength is indicated by line thickness; links color
369 corresponds to the color of brain rhythms involved. Networks include only links with
370 strength above the significance threshold $\%TDS = 2.3\%$. The length of each colored
371 segment along each radius in the radar-charts represents the TDS coupling strength
372 between each cortical rhythm at each EEG location and the leg muscle tone averaged
373 over all EMG bands. Segments in the radar-charts are shown with same color as the

374 corresponding brain rhythms. (B) Characteristic profiles of network links strength for
375 cortical rhythms interactions with integrated leg-muscle tone for right brain hemisphere.
376 Link strengths are grouped by brain areas, and are ordered from low- to high-frequency
377 cortical rhythms. Error bars represent the standard error; horizontal green lines are the
378 significance threshold.

379

380 *Figure 3.* Dynamic networks of leg EMG frequency bands and integrated brain activity
381 at cortical areas for different physiological states. (A) Links in network maps represent
382 group-averaged TDS coupling strength between each frequency band of leg muscle tone
383 and a given cortical area, after averaging network links to all brain waves at the cortical
384 area. Cortical areas are represented by EEG channel locations, while peripheral network
385 nodes with different colors represent leg EMG frequency bands. Line thickness
386 indicates link strength (weak links with $3\% < TDS < 5\%$, intermediate links with $5\% <$
387 $TDS < 7.5\%$ and strong links with $TDS > 7.5\%$); links color corresponds to the color of
388 the leg EMG frequency bands. (B) Characteristic profiles of network links strength
389 representing interactions between integrated brain activity at distinct cortical areas in the
390 right brain hemisphere and individual leg EMG frequency bands. Links are grouped by
391 cortical areas, and are ordered from low- to high-frequency leg EMG bands. Error bars
392 represent standard error for all subjects; horizontal green lines mark the physiologically
393 relevant significance threshold $\%TDS = 2.3\%$.

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